





# Polymeric Composites Based on Carboxymethyl Cellulose Cryogel and Conductive Polymers: Synthesis and Characterization

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**Abstract:** In this study, a super porous polymeric network prepared from a natural polymer, carboxymethyl cellulose (CMC), was used as a scaffold in the preparation of conductive polymers such as poly(Aniline) (PANi), poly(Pyrrole) (PPy), and poly(Thiophene) (PTh). CMC–conductive polymer composites were characterized by Fourier transform infrared (FT-IR) spectroscopy, thermogravimetric analysis (TGA) techniques, and conductivity measurements. The highest conductivity was observed as  $4.36 \times 10^{-4} \pm 4.63 \times 10^{-5}$  S·cm<sup>-1</sup> for CMC–PANi cryogel composite. The changes in conductivity of prepared CMC cryogel and its corresponding PAN, PPy, and PTh composites were tested against HCl and NH<sub>3</sub> vapor. The changes in conductivity values of CMC cryogel upon HCl and NH<sub>3</sub> vapor treatment were found to increase 1.5- and 2-fold, respectively, whereas CMC–PANi composites showed a 143-fold increase in conductivity upon HCl and a 12-fold decrease in conductivity upon NH<sub>3</sub> treatment, suggesting the use of natural polymer–conductive polymer composites as sensor for these gases.

**Keywords:** CMC cryogel; natural polymer–conductive polymer cryogel composite; carboxymethyl cellulose cryogel composites; conductive natural polymer cryogel

## 1. Introduction

Conductive polymers were first synthesized as a new generation of organic materials in the mid-1970s. Although the electrical and optical properties of conductive polymers are similar to metals and organic semiconductors, they have attracted more attention owing to their properties, such as the ease of synthesis and easier processing than metals [1–3]. The synthesis methods for conductive polymers can be divided into two main groups, where the starting material is either a polymer or a monomer. Soluble conductive polymers can be deposited through direct polymer solution spraying, sieve, microcontact printing, probe-based deposition, photolithography, and spin coating. Alternatively, monomers can be polymerized by chemical, electrochemical, or plasma techniques [4–7]. Conductive polymers are widely used in microelectronics industries including photovoltaic devices, light-emitting diodes, electrochromic screens, sensors, and battery technology [8–10]. However, the studies in the 1980s demonstrated that conductive polymers are compatible with many biological molecules, causing a significant increase in the use of polymers for biomedical applications. Many conductive polymers such as poly(Aniline) (PANi) [11,12], poly(Pyrrole) (PPy) [13,14], poly(thiophene) (PTh) [15], and their derivatives [16–18] have been reported as cell and tissue compatible, which was

supported by in vitro and in vivo studies. In addition, the chemical, physical, and electrical properties of conductive polymers can be adapted to particular needs by modification of antibodies, enzymes, and some other biological molecules [19–23].

Many events in the human body, such as neural communication, embryonic development, tissue repair after injury, and heartbeat, among others, are regulated by electrical signals [24]. The components that are electrically active in the human body are the nervous system, heart, and muscles, respectively [25,26]. While the electric is used during the transmission of information between neurons in the nervous system, the muscle cells in the heart produce heartbeats by generating electrical impulses that lead to muscle contraction circulating throughout the organ [25,26]. Besides, some tissues, such as bone marrow, have been shown to use conductivity to regenerate [27]. In this context, studies on the design of electrically conductive materials for biotechnological and biomedical applications have attracted a great deal of attention [28] Conductive polymers have become prominent candidates for materials that can be used in these biotechnological and biomedical fields such as biosensors [29,30], neural electrodes [31,32], bio-activators [33,34], wound healing and controlled release systems [35,36], and tissue scaffolds [37,38], owing to their electrical behavior and biocompatibility [39]. The utilization of conductive polymers in these applications can be augmented further by preparing conductive polymers within super-porous biocompatible cryogels.

In this study, for the first time, in situ synthesis of conductive polymers within natural polymer CMC cryogels is reported. The synthesis of cryogels from natural carboxymethyl cellulose (CMC) polymer by employing cryopolymerization technique was accomplished. Then, the synthesized CMC cryogel was used as a template for in situ synthesis of conductive polymers, PANi, PPy, and PTh for the first time. The prepared CMC–conductive polymer cryogel composites were characterized by means of Fourier transform infrared (FT-IR), thermogravimetric analysis (TGA), and conductivity measurements employing an electrometer. Moreover, the changes in the conductivity of CMC, CMC–PANi, CMC–PPy, and CMC–PTh cryogel composites were investigated for the detection of HCl and NH<sub>3</sub> vapor as potential sensing materials.

## 2. Materials and Methods

#### 2.1. Materials

Carboxymethyl cellulose sodium (CMC,  $M_w \sim 250,000$ , degree of substitution: 1.2, Aldrich, St. Louis, MO, USA), divinyl sulfone (DVS, 98%, Merck, Kenilworth, NJ, USA), aniline (ANi, 99%, Sigma-Aldrich, St. Louis, MO, USA), pyrrole (Py, 98%, Aldrich), thiophene (Th, 99%, Aldrich), ammonium persulfate (APS, 98%, Sigma-Aldrich), Iron (III) chloride (FeCl3, 98%, Fluka), hydrochloric acid (HCl, 37%, VWR Chemicals, Radnor, PA, USA), sodium hydroxide (NaOH, 98.8%, VWR Chemicals), chloroform (CH<sub>3</sub>Cl, 99%, Riedel de Haen), ethanol (99.8%, Sigma-Aldrich), hydrochloric acid (HCl, 37%, VWR Chemicals), ammonium solution (NH3, 25%, Sigma Aldrich), and double distilled water (DDW, GFL2108) were used as received.

## 2.2. Synthesis of CMC Cryogel

The synthesis of CMC cryogel was reported earlier [40]. In brief, 0.2 g of CMC was dissolved in 6 mL 0.2 M NaOH under constant stirring at 500 rpm for 4 h at ambient temperature, and then cooled in a freezer about 5 min. Then, DVS crosslinker, with a mole ratio of 100% relative to the CMC repeating unit, was added and quickly pipetted (0.8 cm diameter). The mixture was then placed in a freezer at -18 °C for cryopolymerization reaction for 24 h to complete cryo-crosslinking. Prepared CMC cryogels were cut in similar shapes and washed with DDW for purification. Purified CMC cryogels were dried in a freeze-dryer and stored in closed tubes for further use.

#### 2.3. In Situ Synthesis of Conductive Polymers within CMC Cryogels

For in situ synthesis of poly(Aniline) (PANi) within CMC cryogels, a similar procedure reported in the literature was followed [41,42]. In short, 0.1 g CMC cryogels were placed in 10 mL ANi monomer for 2 h to load ANi monomer into CMC cryogels at a 100 rpm mxing rate at an ambient temperature. After that, the ANi monomer containing CMC cryogels were weighed, and the amount of loaded ANi was gravimetrically calculated. Then, ANi-loaded CMC cryogels were transferred in 200 mL 1 M HCl containing APS at 1:1.25 APS/ANi mole ratio according to the amount of ANi loaded into the CMC cryogel and stirred at 250 rpm for 30 min. Then, the prepared CMC–PANi cryogel conductive polymer composites were washed with DDW and ethanol, and dried in an oven at 50 °C.

In situ synthesis of poly(Pyrrole) (PPy) within CMC cryogels was also carried out in a similar procedure with some modification [41,42]. CMC cryogels weighing 0.1 g were placed in 10 mL Py monomer to load Py into CMC cryogels. Then, the Py-loaded CMC cryogels were placed into 0.05 M 250 mL FeCl<sub>3</sub> solution in DDW and stirred at 250 rpm for 2 h at an ambient temperature for in situ polymerization of Py within CMC cryogels. Then, the prepared CMC-PPy cryogel conductive polymer composites were washed with DDW and ethanol, and dried in an oven at 50 °C.

The synthesis procedure of poly(Thiophene) (PTh) within CMC cryogels was also done based on a previously reported method [41,42]. Briefly, CMC cryogels weighing 0.1 g were placed in 10 mL of Th monomer to load Th into CMC cryogels. After that, Th loaded CMC cryogels were placed into 50 mL 0.03 M FeCl<sub>3</sub> solution in chloroform and placed in an oil bath at 65 °C with reflux system, and stirred at 250 rpm for 16 h for the polymerization of Th within CMC cryogels. Finally, the prepared CMC–PTh cryogel conductive polymer composites were washed with DDW and ethanol, and dried in an oven at 50 °C.

## 2.4. Characterization

The characterization of synthesized CMC cryogels and conductive polymer composites was done using Fourier transform infrared (FT-IR) spectrometer (Nicolet iS10, Thermo, Waltham, MA, USA), thermogravimetric analyzer (TGA, SII 6300, Exstar, Stoneham, MA, USA), and an electrometer (2400 Source-meter, Keithley, Cleveland, OH, USA) for conductivity measurements.

#### 2.5. Conductivity Measurements

Conductivity of synthesized CMC cryogels and their corresponding PANi, PPy, and PTh composites was measured from the ohmic region of current–voltage (I–V) curves constructed from an electrometer using Equations (1) and (2):

$$V = I \times R \tag{1}$$

$$\sigma = (1/R) \times (l/A) \tag{2}$$

where 'V' is the voltage, 'I' is the current, 'R' is the bulk resistance, ' $\sigma$ ' is the conductivity, '1/R' is the resistivity, 'I' is the thickness, and 'A' is the cross-sectional area of the sample.

In the conductivity measurements, small pieces of conductive carbon tapes (3 mm  $\times$  4 mm) were attached at the top and bottom sides of CMC cryogels and/or CMC–conductive polymer composites, and then the electrodes of the electrometer were contacted with these carbon tapes. Next, the I–V curves were obtained by applying voltages up to 100 V to determine the conductivity of the samples.

#### 3. Results and Discussion

#### 3.1. Synthesis and Characterization of In Situ Synthesized Conductive Polymer CMC Cryogel Composites

The well-known cryo-crosslinking technique was used in the preparation of CMC cryogels having an interconnected super macroporous structure. Scanning Electron Microscopy (SEM) images of CMC cryogels synthesized using 100% DVS crosslinker based on the repeating unit of CMC were previously reported by our group reporting the super macroporous structure of CMC cryogels with a pore size in a range of 1–100  $\mu$ m [40]. Recently, the synthesis of conductive polymers within cryogels was reported [41,42]. The schematic presentation of in situ synthesis of conductive polymers within CMC cryogels is given in Figure 1a–c for PANi, PPy, and PTh synthesis, respectively. Briefly, 0.1 g of purified cylindrical CMC cryogel pieces was placed into ANi, Py, and Th monomers separately about 2 h for loading of monomers into CMC cryogels. Then, depending on monomer, the conductive monomer-loaded CMC cryogels were placed into the appropriate initiator solution, as described above.



**Figure 1.** The schemcatic presentation of in situ synthesis of (**a**) poly(Aniline) (PANi), (**b**) poly(Pyrrole) (PPy), and (**c**) poly(Thiophene) (PTh) conductive polymers within carboxymethyl cellulose (CMC) cryogels. APS, ammonium persulfate.

As a result of in situ synthesis of conductive polymer, the interconnected super macro pores of CMC cryogels were filled with PANi or PPy, or PTh, as shown in Figure 1. The amounts of loaded ANi, Py, and Th into CMC cryogels; the amounts of in situ synthesized conductive polymers within CMC cryogels; and in situ polymerization efficiency of conductive polymers within CMC cryogels are summarized in Table 1. The ANi, Py, and Th loaded CMC cryogels were weighed and the amount of incorporation of each ANi, Py, and Th monomer into CMC structure is calculated. Briefly, cryogels of known weight were placed in monomers and weighed again to calculate the loaded amount of the corresponding monomers.

<b>Table 1.</b> The amount of loaded Aniline (ANi), Pyrrole (Py), and Thiophene (Th); the amount of in situ
synthesized cryogel composites; and in situ polymerization yield. CMC, carboxymethyl cellulose.

Materials (Cryogel Composite)	Weigth of CMC Cryogels (g)	Loaded Amount of Monomer (g)	Amount of Composite Cryogel (g)	Yield of In Situ Polymerization (%)
CMC-PANi	$0.1 \pm 0.01$	$1.98\pm0.02$	$0.97 \pm 0.11$	$46.2 \pm 5.44$
CMC-PPy	$0.1 \pm 0.01$	$1.94 \pm 0.03$	$0.23 \pm 0.01$	$10.9\pm0.21$
CMC-PTh	$0.1\pm0.01$	$1.92\pm0.03$	$0.11\pm0.01$	$5.18 \pm 0.49$

In brief, the weight of known cryogel was placed into monomers of the desired conductive polymer and weighted again to calculate the loaded amount of the corresponding monomers. The amounts of in situ prepared conductive polymers were then calculated from the weight of the cryogel–conductive polymer composites. The percent yield of in situ polymerized conductive polymers was calculated from the amount of in situ polymerized conductive polymers and loaded amount of monomer. Upon polymerization of ANi, Py, and Th within CMC cryogels by placing into corresponding solutions for the in situ synthesis of conductive PANi, PPy, and PTh polymers within CMC cryogels, the weights of conductive PANi, PPy, and PTh polymers were computed as  $0.97 \pm 0.11$ ,  $0.23 \pm 0.01$ , and  $0.11 \pm 0.01$  g, respectively. The in situ polymerization efficiency of conductive PANi, PPy, and PTh within CMC cryogels was gravimetrically assessed as  $46.21\% \pm 5.44\%$ ,  $10.95\% \pm 0.21\%$ , and  $5.18\% \pm 0.49\%$ , respectively.

The FT-IR spectra and TGA thermograms of CMC cryogel, as well as CMC–PANi, CMC–PPy, and CMC–PTh composites, are shown in Figure 2a,b, respectively. In Figure 2a, the FT-IR spectrum of CMC cryogels gave characteristic peaks as wide band around 3350 cm<sup>-1</sup> assigned to –OH stretching, asymmetric stretching of –COO- at 1592 cm<sup>-1</sup>, symmetric stretching of -COO- at 1423 cm<sup>-1</sup>, and –CO stretching at 1047 cm<sup>-1</sup>, respectively. On the other hand, new bands appeared at 1544 cm<sup>-1</sup> corresponding to benzenoic-quinonic nitrogen, at 1494 cm<sup>-1</sup> for aromatic C-C, at 1288 cm<sup>-1</sup> for aromatic amine group, and at 1118 cm<sup>-1</sup> for C-N-C stretching in the FT-IR spectrum of CMC–PANi cryogel composites, which are in accordance with the literature [43]. The characteristic bands of PPy were also observed in the FT-IR spectrum of CMC–PPy cryogel composites at 1358 cm<sup>-1</sup> corresponding to the presence of polymerized pyrrole units [44]. Moreover, the peaks observed at 703, 1319, and 1426 cm<sup>-1</sup> from the FT-IR spectrum of CMC–PTh cryogel composites were assigned to  $\alpha$ - $\alpha$  connection between thiophene molecules [45], and C-H in-plane bending vibrations of Th molecules, respectively [46].



**Figure 2.** (**a**) Fourier transform infrared (FT-IR) spectrum and (**b**) thermogravimetric analysis (TGA) thermograms of CMC cryogel, CMC–PANi, CMC–PPy, and CMC–PTh cryogel composites.

The thermal stability and degradation steps of CMC cryogel, CMC–PANi, CMC–PPy, and CMC–PTh cryogel composites were compared with TGA analysis and corresponding TGA thermograms are given in Figure 2b. The first degradation step of CMC cryogel was observed between 260 and 308 °C with 41.5% weight loss from the thermogram, the second step of degradation was

observed between 676 and 694 °C with 75.8% weight loss, and 78.8% weight loss was observed at 800 °C. On the other hand, it was deduced that the thermal stability of CMC cryogels decreased with the in situ synthesis of PANi conductive polymer, where the first degradation step was seen between 137 and 208 °C with 43.1% weight loss, the second step of degradation was observed between 425 and 607 °C with 89.8% weight loss, and 91.2% weight loss was attained at 800 °C from the TGA thermogram of the CMC–PANi cryogel composite. The one step degradation of CMC–PPy cryogel composites was noticed between 224 and 517 °C with 91.2% weight loss, and 92.1% weight loss was observed at 800 °C. Finally, the TGA thermogram of CMC–PTh cryogel composites also resulted in two degradation steps, starting between 222 and 278 °C with 16.5% weight loss, between 373 and 414 °C with 58.5% weight loss, and 63.8% weight loss was observed at 800 °C. TGA thermograms of CMC cryogel, CMC–PANi, CMC–PPy, and CMC–PTh cryogel composites clearly show that the thermal stability of CMC cryogel decreased by in situ synthesis of PANi, and slightly decreased for the in situ synthesis of PPy and PTh conductive polymers.

## 3.2. Conductivity Measurements

Although the reason behind the conductivity for conjugated organic molecules was initially assumed to be derived from unfilled electronic valence and conduction bands, it was later shown that the conductivity can be associated with spineless charge carriers such as soliton, polaron, and bipolaron, after the discovery of conductive polymers such as PANi, PPy, and PTh [47]. In this study, the conductivity of CMC cryogels, as well as the changes in conductivities of CMC–PANi, CMC–PPy, and CMC–PTh cryogel composites, were determined by using an electrometer from the ohmic region of obtained I–V curves. In Figure 3a, the digital camera images of CMC cryogel, CMC–PANi, CMC–PPy, and CMC–PTh cryogel composites are given. It was clearly seen that the white color of CMC cryogels turned to black after in situ synthesis of PANi and PPy, and also turned to light brown upon in situ synthesis of PTh conductive polymer.



**Figure 3.** (**a**) Digital camera images of synthesized CMC cryogel, CMC–PANi, CMC–PPy, and CMC–PTh cryogel composites; and (**b**) schematic representation of electrometer measurement.

The schematic representation of electrometer measurement setup is shown in Figure 3b. As can be seen, the probes of electrometer were contacted to carbon tapes that were attached at the top and

bottom sides of CMC-based cryogels and cryogel composites. The corresponding I–V curves of CMC cryogel, CMC–PANi, CMC–PPy, and CMC–PTh are given in Figure 4a.



**Figure 4.** The comparison of (**a**) current–voltage (I–V) curves obtained from electrometer; and (**b**) calculated conductivity values of CMC cryogel, CMC–PANi, CMC–PPy, and CMC–PTh cryogel composites.

The conductivity values were calculated from I–V curves using Equations (1) and (2), and are illustrated in Figure 4b for CMC cryogel, CMC–PANi, CMC–PPy, and CMC–PTh cryogel composites. The conductivity of CMC cryogels was calculated as  $2.21 \times 10^{-9} \pm 1.98 \times 10^{-10}$  S·cm<sup>-1</sup>. An approximately 200 K-fold increase was observed in the conductivity of CMC cryogels by the in situ synthesis of PANi, which was calculated as  $4.58 \times 10^{-4} \pm 5.68 \times 10^{-5}$  S·cm<sup>-1</sup>. The conductivity of CMC–PPy cryogel composites was calculated as  $5.02 \times 10^{-5} \pm 5.54 \times 10^{-6}$  S·cm<sup>-1</sup> with approximately a 25 K-fold increase as compared with the conductivity of bare CMC cryogel. On the other hand, the difference between conductivity value of CMC–PTh cryogel composites was insignificant, where the calculated conductivity value of CMC–PTh cryogel composites was 2.28  $\times 10^{-9} \pm 5.24 \times 10^{-10}$  S·cm<sup>-1</sup>. Among the monomers used for in situ syntheses of conductive polymers within CMC cryogel, Th polymerization stands out as the most difficult one. The results summarized in Table 1 confirm this phenomenon as the in situ polymerization efficiency for PTh within CMC cryogels was calculated as 5%. Therefore, the observation of some major differences in conductivity values among the conductive polymers and CMC–PTh cryogel composites can be explained by a very small amount of PTh conductive polymer in CMC cryogels.

The highest increase in conductivity was observed after in situ synthesis of PANi with a 200 K-fold increase, following Py with a 25 K-fold increase, which could be owing to their higher amounts within CMC pores, allowing better conductivity.

#### 3.3. The Change in Conductivity Upon Exposure to HCl and NH<sub>3</sub> Vapors

The potential sensor use of the prepared CMC cryogel, CMC-PANi, CMC-PPy, and CMC-PTh cryogel composites for HCl and NH<sub>3</sub> vapors was tested by measuring the changes in conductivities of prepared CMC-based cryogels by following literature [41]. In brief, CMC cryogel, CMC-PANi, CMC–PPy, and CMC–PTh cryogel composites were treated with HCl and NH<sub>3</sub> vapors for 15 min by employing a simple experimental set up [41]. Cryogel composites were exposed to HCl and NH<sub>3</sub> vapors using a simple set up. In brief, two funnels were connected with a glass fritted neck, where cryogel composites were placed on the top surface of the glass frit connected with another funnel containing a glass cotton that is attached to HCl or NH<sub>3</sub> solutions with a valve for the release of vapors. The conductivities of CMC cryogel, CMC-PANi, CMC-PPy, and CMC-PTh cryogel composites were calculated before and after gas exposures. The conductivity changes in CMC cryogel, CMC-PANi, CMC-PPy, and CMC-PTh cryogel composites after treating with HCl vapor for 15 min are demonstrated in Figure 5a, and the values are summarized in Table 2. The conductivity of CMC cryogel was increased from  $2.31 \times 10^{-9} \pm 2.19 \times 10^{-10}$  S·cm<sup>-1</sup> to  $4.59 \times 10^{-9} \pm 6.33 \times 10^{-10}$ S·cm<sup>-1</sup> with approximately a twofold increase after 15 min of HCl vapor treatment. Moreover, the conductivity of CMC–PANi cryogel composite increased from  $4.36 \times 10^{-4} \pm 4.63 \times 10^{-5}$  S·cm<sup>-1</sup> to  $6.24 \times 10^{-2} \pm 5.21 \times 10^{-3}$  S·cm<sup>-1</sup> with approximately a 150-fold increase after 15 min of HCl vapor treatment. Further, the conductivity of CMC–PTh was increased from  $2.12 \times 10^{-9} \pm 8.36 \times 10^{-9}$  S·cm<sup>-1</sup> to  $3.67 \times 10^{-8} \pm 3.36 \times 10^{-9}$  S·cm<sup>-1</sup> with approximately a 20-fold increase after 15 min of HCl vapor treatment. The change in conductivity of CMC-PPy was found to be insignificant as the conductivity was increased to  $5.97 \times 10^{-5} \pm 9.32 \times 10^{-6}$  S.cm<sup>-1</sup> from  $4.98 \times 10^{-5} \pm 3.57 \times 10^{-6}$  S·cm<sup>-1</sup>. Overall, the highest conductivity change was observed for CMC-PANi cryogels with a 150-fold increases after HCl vapor treating for 15 min. As HCl was also used for the in situ synthesis of PANi within CMC cryogels, this conductivity increase in the CMC-PANi cryogel composite can be explained by the further doping effect of HCl vapor for PANi conductive polymers within the CMC superporous network.



**Figure 5.** The change in the conductivities of CMC cryogel, CMC–PANi, CMC–PPy, and CMC–PTh cryogel composites after 15 min (**a**) HCl and (**b**) NH<sub>3</sub> vapor exposure.

Materials	Conductivity (S·cm <sup>-1</sup> )						
	HCl Vapor		Change	NH <sub>3</sub> Vapor		Change	
	Before	After	(fold)	Before	After	(fold)	
СМС	$2.31 \times 10^{-9}$	$4.59 \times 10^{-9}$	2	$2.16 \times 10^{-9}$	$3.11 \times 10^{-9}$	1.5	
CMC-PANi	$4.36 \times 10^{-4}$	$6.24 \times 10^{-2}$	143	$4.11\times10^{-4}$	$3.27 \times 10^{-5}$	12	
CMC-PPy	$4.98  imes 10^{-5}$	$5.97  imes 10^{-5}$	1.2	$5.16 \times 10^{-5}$	$1.11\times10^{-5}$	5	
CMC-PTh	$2.12 \times 10^{-9}$	$3.67 \times 10^{-8}$	17	$2.51 \times 10^{-9}$	$4.14\times10^{-8}$	16	

**Table 2.** The changes in the conductivities of CMC cryogel, CMC–PAN, CMC–PPY, and CMC–PTh cryogel composites after 15 min HCl and NH<sub>3</sub> vapor treatment.

The conductivity changes in CMC cryogel, CMC–PANi, CMC–PPy, and CMC–PTh cryogel composites after treating with NH<sub>3</sub> vapor for 15 min are shown in Figure 5b. As shown in Table 2, the conductivity changes in CMC cryogel, CMC–PANi, CMC–PPy, and CMC–PTh cryogel composites are from  $2.16 \times 10^{-9} \pm 3.71 \times 10^{-10}$  S·cm<sup>-1</sup> to  $3.11 \times 10^{-9} \pm 5.95 \times 10^{-10}$  S·cm<sup>-1</sup>, from  $4.11 \times 10^{-4} \pm 5.32 \times 10^{-5}$  S·cm<sup>-1</sup> to  $3.27 \times 10^{-5} \pm 2.56 \times 10^{-5}$  S·cm<sup>-1</sup>, from  $5.16 \times 10^{-5} \pm 4.38 \times 10^{-6}$  S·cm<sup>-1</sup> to  $1.11 \times 10^{-5} \pm 8.73 \times 10^{-6}$  S·cm<sup>-1</sup>, and from  $2.51 \times 10^{-9} \pm 9.17 \times 10^{-10}$  S·cm<sup>-1</sup> to  $4.14 \times 10^{-8} \pm 4.28 \times 10^{-9}$  S·cm<sup>-1</sup>, respectively. The highest conductivity change was observed for the CMC–PTh cryogel composite with a 15-fold increase upon 15 min NH<sub>3</sub> vapor treatment. Besides, 12-fold and 5-fold decreases were observed in the conductivity of CMC–PANi and CMC–PPy cryogel composites, respectively.

As a consequence, it can be assumed that the amounts of conductive polymer in CMC cryogel templates and the types of conductive polymer can affect the potential sensor applications of composite systems against different gases, for example, HCl and NH<sub>3</sub> vapor.

## 4. Conclusions

Herein, CMC cryogels from natural sources were utilized as a template for in situ PANi, PPy, and PTh conductive polymer synthesis for the first time in the literature. It was observed that the conductivity of CMC cryogels was increased by in situ preparation of PANi and PPy conductive polymers to  $4.36 \times 10^{-4} \pm 4.63 \times 10^{-5}$  S·cm<sup>-1</sup> with a 200 K-fold increase, and  $4.98 \times 10^{-5} \pm 3.57 \times 10^{-5}$ 10<sup>-6</sup> S·cm<sup>-1</sup> with approximately a 25 K-fold increase according to conductivity of CMC cryogels, respectively. The potential sensor application of CMC-based PANi, PPy, and PTh cryogel composites was also tested against HCl and NH<sub>3</sub> vapor exposure. The most significant conductivity difference was realized for CMC-PANi cryogel against HCl vapor by 15 min exposure time, with a 150-fold increase in the conductivity attributed to the doping of PANi conductive polymers with HCl vapor. Additionally, a 15-fold increase was observed in the conductivity of CMC-PTh, and a 12-fold decrease was observed in the conductivity of CMC-PANi against NH<sub>3</sub> vapor exposure by 15 min exposure. Overall, it can be concluded that CMC-PANi, CMC-PPY, and CMC-PTh cryogel composites can be used as a sensor for HCl and NH<sub>3</sub> vapors. Importantly, the innate biocompatibility of CMC cryogels, and sustainability of CMC with the capability of in situ prepared PANi, PPY, and PTh conductive polymers, make these natural-synthetic polymer composites promising materials for biotechnological and biomedical applications.

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