Research Article

A Novel Anti-HIV Dextrin–Zidovudine Conjugate Improving the Pharmacokinetics of Zidovudine in Rats

Sumalee Wannachaiyasit,¹ Pithi Chanvorachote,² and Ubonthip Nimmannit^{1,3}

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Abstract. The aim of this study was to investigate a newly synthesized dextrin–zidovudine (AZT) conjugate designed as a sustained release prodrug of AZT for parenteral administration. AZT was first reacted with succinic anhydride to form a succinoylated AZT which was subsequently coupled with dextrin to yield the dextrin–AZT conjugate. The structure of the conjugate was characterized by FT-IR and ¹H-NMR spectroscopy. The drug content of the conjugate was 18.9 wt.%. The release *in vitro* of free AZT and succinoylated AZT was investigated in buffer solutions at pH 5.5 and 7.4 and in human plasma. AZT and succinoylated AZT release from the conjugate was 1.4% (pH 5.5), 41.7% (pH 7.4) and 78.4% in human plasma after 24 h. Release was complete in human plasma after 48 h. A pharmacokinetic study in rats following intravenous administration of the conjugate showed prolonged plasma levels of AZT compared to free AZT. The use of the conjugate extended the plasma half-life of AZT from 1.3 to 19.3 h and the mean residence time from 0.4 to 23.6 h. Furthermore, the conjugate provided a significant greater area under the plasma concentration-time curve and reduced the systemic clearance of AZT. This study suggested the potential of this novel dextrin–AZT conjugate as a new intravenous preparation of AZT.

KEY WORDS: AZT; dextrin; polymeric prodrug; sustained release; zidovudine.

INTRODUCTION

Zidovudine (AZT) was the first clinically approved nucleoside reverse transcriptase inhibitor widely used for the treatment of acquired immunodeficiency syndrome (AIDS) caused by the human immunodeficiency virus (HIV). It has been used in many anti-HIV combination therapies including the suppression of HIV transmission from mother to fetus and the post-exposure prophylaxis of healthcare workers following exposure to HIV (1–8).

The clinical limitations of AZT are its short plasma halflife (approximately 1 h), and its dose-dependent toxicities (9,10), especially granulocytopenia and anemia, often found in AZT-treated patients (11–13). Its short plasma half-life demands frequent administration of high doses to maintain therapeutic drug levels. Current oral and intravenous (I.V.) AZT dosage forms lead to fluctuations of plasma drug concentration with an initial high concentration that increases the risk of hematological toxicities, and subsequent low drug levels that are below the therapeutic threshold. Oral dosage forms have the disadvantage that AZT undergoes extensive first pass metabolism thus only 64% of the dose reaches

virus infusion. It is infused into the vein over 1 h six times a day (every 4 h) at a dose of 1–2 mg/kg body weight. After injection, it is rapidly excreted in the urine as metabolized and unchanged forms (16). There is no sustained release I.V. preparation of AZT available on the market. In our research, a sustained release I.V. dosage form of AZT was formed to reduce the frequency of administration. The sustained release of AZT may allow dose reduction and smaller fluctuations in drug levels, using here the strategy of a polymer–drug conjugate (a polymeric AZT prodrug).
(I.V.) Polymer–drug conjugates employ a water soluble, polymeric carrier as a platform to covalently bind drugs via a spacer which is designed to allow drug release through simple hydrolysis or enzymatic cleavage (17–21). Ideal polymeric carriers are water-soluble, non-toxic, non-immunogenic, eas-

blood circulation (13,14) and the absorption of AZT from gastrointestinal tract is variable patient to patient (15). I.V.

therapy is used in patients that cannot receive oral medica-

tion, such as pregnant women during labor and delivery (16).

The available I.V. preparation is in the form of solution for

ily chemical manipulated and available at low cost (22). Dextrin is a promising polymer as it has these characteristics. It is biodegradable so it does not accumulate in long-term use. It has been already used clinically as a peritoneal dialysis solution (23–25). Dextrin is a natural, water-soluble, linear polymeric carrier containing primarily α -1,4 linkages with small amounts of branching α -1,6 linkages prepared by acid or enzymatic hydrolysis of starch (23,26). Its chemical structure is also suitable for conjugation with drugs as it has hydroxyl groups, providing reaction sites that can be used to

¹ Pharmaceutical Technology (International) Program, Faculty of Pharmaceutical Sciences, Chulalongkorn University, Pathumwan, Bangkok 10330, Thailand.

² Department of Physiology, Faculty of Pharmaceutical Sciences, Chulalongkorn University, Pathumwan, Bangkok 10330, Thailand.

³ To whom correspondence should be addressed. (e-mail: nubonthi@ chula.ac.th)

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attach bioactive molecules. Dextrin modified by attachment of sulfate groups at its hydroxyl groups (sulfated dextrin) has anti-HIV activity and anti-coagulant activity which results in thrombocytopenia, an increase in bleeding time and a decrease in platelet count, toxicities that limit the use of sulfated dextrin (and other sulfated polysaccharides) by the I. V. route (27–29). Studies in HIV-infected patients showed the failure of I.V. sulfated dextran to reduce viral titer (serum p24 levels) and the high toxicity was unacceptable (29). As a consequence we used non-sulfated dextrin for conjugation with AZT.

Our aim was to investigate a new dextrin–AZT conjugate for prolonging AZT blood levels and improving the pharmacokinetics of AZT. A dextrin–AZT conjugate was synthesized and characterized. The *in vitro* drug release was determined in buffer solutions at pH 5.5 and 7.4 chosen to mimic the intracellular and extracellular pH, and in human plasma. The hemolytic activity of the dextrin–AZT conjugate was examined to judge the safety of the conjugate. The pharmacokinetic study in rats compared the dextrin–AZT conjugate and free drug following I.V. administration.

MATERIALS AND METHODS

Materials

AZT originated from Samchully Pharmaceuticals (Seoul, South Korea) and was obtained from The Government Pharmaceutical Organization, Bangkok, Thailand. Dextrin (weight-average molecular weight of 6,600 g/mol with the weight-average molecular weight to number-average molecular weight ratio being 1.8, determined by gel permeation chromatography), 4-dimethylaminopyridine (DMAP), dry tetrahydrofuran (THF), poly(ethyleneimine) (PEI), dextran and phosphate buffered saline (PBS) were purchased from Sigma Chemical (St. Louis, MO, USA). Succinic anhydride was purchased from Aldrich Chemical (Milwaukee, Wl, USA). N, N'-dicyclohexylcarbodiimide (DCC) was from Merck (Hohenbrunn, Germany). 1-Hydroxybenzotriazole (HOBt) was from Epochem (Shanghai, China). Triethylamine was from Carlo Erba Reagent (Rodano, MI). Dry N, N'-dimethylformamide (DMF) and dry dimethylsulfoxide (DMSO) were from Sigma-Aldrich Chemicals (Steinheim, Germany). 2, 5-Dihydroxybenzoic acid (DHB) was from Bruker Daltonics (Leipzig, Germany). Methanol (HPLC grade) and acetonitrile (HPLC grade) were from Fisher Scientific UK (Leicestershire, UK). Citric acid and di-sodium hydrogen orthophosphate (Na₂HPO₄) were from Ajax Finechem (Auckland, New Zealand). SpectraPor membranes (MWCO=2,000) were obtained from Spectrum Laboratories (Dominguez, CA, USA). Sephadex LH-20 was from Amersham Biosciences (Uppsala, Sweden). All other chemicals and solvents were analytical grade. Human blood and plasma of healthy volunteer blood donors were supplied by the Thai Red Cross Society (Bangkok, Thailand). The protocol was approved by the Ethics Committee of Chulalongkorn University.

Synthesis of Succinoylated AZT

Succinoylated AZT was synthesized by a modification of the reported method (30). Briefly, AZT (1.976 mmol) was reacted with succinic anhydride (3.163 mmol) in the presence of triethylamine (2.570 mmol) in 25 ml of dry THF at 69°C. The progress of reaction was followed by thin layer chromatography (TLC) (chloroform/methanol, 9:1, vol/vol) and after 6 h, succinic anhydride (0.988 mmol) and triethylamine (1.383 mmol) were added again and the reaction was left at 69°C for 6 h. After reaction, the solvent was evaporated and the residue was dissolved in distilled water (50 ml) and then adjusted to pH 2 by 1M HCl. The solution was transferred to a separating funnel and extracted with ethyl acetate several times. The ethyl acetate phase was collected and dried over anhydrous sodium sulfate overnight. The organic phase was filtered and evaporated. The residue was purified by flash column packed with Sephadex LH-20 and eluted with mixed solvent (chloroform/methanol, 9:1, vol/vol) (yield ~80%). The white residue was characterized by Fourier transforminfrared spectroscopy (FT-IR) (Perkin Elmer FT-IR Spectrometer Spectrum 2000) and ¹H nuclear magnetic resonance spectroscopy (¹H-NMR) (Avance DPX-400 at 400 MHz spectrometer).

Synthesis of the Dextrin-AZT Conjugate

Dextrin (0.976 mmol) was dissolved in 17 ml of dry DMF and 3 ml of dry DMSO at 50°C with agitation overnight. The solution of succinoylated AZT (0.391 mmol) and DCC (1.562 mmol) in 10 ml of dry DMF was stirred for 15 min under nitrogen. The solution of HOBt (1.172 mmol) in 4 ml of dry DMF was added and the reaction was left for 30 min. The overnight-prepared dextrin solution and DMAP (0.976 mmol) were added to the reaction mixture. The reaction was left at room temperature, with stirring under nitrogen for 48 h. The precipitate of dicyclohexylurea was then filtered, the filtrate collected and the solvent removed and the residue precipitated in vigorously stirring diethyl ether. The precipitate was collected and dissolved in distilled water (50 ml). The impurity was successively extracted with ethyl acetate (4×40 ml) and chloroform (4×40 ml). The aqueous phase was then dialyzed against distilled water. The dextrin-AZT conjugate solution was dried using a freezedrying technique (yield 87%). The white residue was characterized by FT-IR, ¹H-NMR and matrix-assisted laser desorption/ionization time-of-flight mass spectroscopy (MALDI-TOF-MS). The percentage molar content of linked AZT was estimated by UV and ¹H-NMR. For UV analysis, the calibration curve of AZT was used to calculate AZT loading. For ¹H-NMR analysis, the integrated signals of anomeric protons of dextrin at 4.60 to 5.45 ppm (as internal reference signal) were compared with the signals of protons of AZT at 1.66 ppm (CH₃-C5), 5.94 ppm (H-C1') and 7.28 ppm (H-C6). One unit of dextrin monomer contains one anomeric proton, therefore the ratio of anomeric proton of dextrin to observed protons of AZT is 1:5. The calculation from ¹H-NMR analysis follows (Eq. 1):

Mol% of linked AZT =
$$(x/5y) \times 100$$
 (1)

where x is the sum of the integrated areas of protons of AZT at 1.66 ppm (CH₃-C5), 5.94 ppm (H–C1') and 7.28 ppm (H–C6) and y is the integrated area of anomeric protons of dextrin at 4.60 to 5.45 ppm.

MALDI-TOF-MS Analysis

Dextrin or the dextrin–AZT conjugate (0.5 mg) was dissolved in 1 ml of nanopure water as a sample solution. A saturated solution of 2, 5-dihydroxybenzoic acid (DHB) prepared in acetonitrile: water (1:1, vol/vol) was used as a matrix solution. The sample solution (1 μ l) was mixed with the matrix solution (5 μ l). An aliquot of the mixture solution (1 μ l) was then deposited on an MTP AnchorChip target (Bruker Daltonics) and air-dried. Samples were analyzed using a Reflex IV MALDI-TOF mass spectrometer (Bruker Daltonics) equipped with delayed extraction, a 2 GHz LeCroy digitizer and a 337 nm nitrogen laser. The instrument was operated in linear and negative ion mode. The accelerating potential was 20 kV.

HPLC Analysis

High-performance liquid chromatography (HPLC) analysis was conducted with a Shimadzu instrument (Model LC-10AD VP), equipped with a Shimadzu (Model SPD-10A VP) variable-wavelength UV detector. The analytical column was a reversed phase C-18 (ODS-3, 250×4.6 mm i.d., particle size 5 µm, from Inersil) connected to a C-18 guard column.

The mobile phase system for quantification of AZT and succinoylated AZT consisted of components A and B. Mobile phase A was 0.01% (vol/vol) ortho-phosphoric acid in water and mobile phase B was a mixture of acetonitrile: methanol (1:1, vol/vol). A gradient elution program was used, at 0 to 14 min, mobile phase A was fixed at 93% with a linear increase in flow rate from 1.5 to 2 ml/min. At 14th min, the mobile phase B was increased immediately from 7% to 22% and then linearly increased up to 40% at the 28th min. After 28 min, mobile phase A was returned to 93% with a flow rate of 1.5 ml/min for 7 min to re-equilibrate the column. A UV

detector was used and fixed at 266 nm. Stavudine (165 μ g/ml) was used as an internal standard.

Calibration curves for AZT were prepared using a concentration range of $0.12-37.17 \mu$ g/ml. The stavudine standard (60 µl) was added into the AZT standard solutions (720 µl) with final AZT concentrations of $0.12-37.17 \mu$ g/ml. Aliquots of these solutions (10 µl) were injected onto the HPLC, and the peak area ratio of AZT/stavudine determined. The calibration curves for succinoylated AZT were created using the same method over a concentration range of $0.11-549.23 \mu$ g/ml.

Calibration curves for AZT and succinoylated AZT were also prepared in plasma. Human plasma (650 μ l) in a microcentrifuge tube was spiked with AZT standard solutions (100 μ l) and the stavudine internal standard (75 μ l). The mixture was mixed, and then 20% (wt/vol) of trichloroacetic acid (150 μ l) was added. The tubes were vortexed for 30 s and then centrifuged at 12,000 rpm for 7 min to obtain a clear supernatant. The final concentrations of AZT ranged from 0.02 to 40.40 μ g/ml. An aliquot of the supernatant (10 μ l) was then injected onto the HPLC. For succinoylated AZT, a calibration curve was prepared using the same method but over the concentration range of 0.03–103.08 μ g/ml.

The HPLC method for AZT and succinoylated AZT was validated following ICH (Q2B) guidelines (31). AZT and succinoylated AZT in plasma were prepared in the range of $0.02-40.40 \mu g/ml$ and $0.03-103.08 \mu g/ml$, respectively. Linearity was evaluated by linear regression analysis of the plot between the peak area ratios of AZT/stavudine or succinoylated AZT/stavudine and sample concentrations. Accuracy was determined as percent recovery. The percent recovery of AZT from plasma was performed using three replicates of three different concentrations of 6.73, 13.47 and 40.40 $\mu g/ml$ and succinoylated AZT was assayed at concentrations of 2.58, 20.62 and 82.46 $\mu g/ml$. The percent recovery was determined



Fig. 1. Synthesis of succinoylated a AZT and b the dextrin-AZT conjugate

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by comparing observed concentrations with actual concentrations. Intra-day precision of AZT or succinovlated AZT was determined by analyzing six replicates of three different concentrations of AZT (8.08, 20.20 and 40.40 µg/ml) or succinoylated AZT (5.15, 34.36 and 82.46 µg/ml) in plasma within the same day. For inter-day precision, three replicates of corresponding concentrations of AZT or succinoylated AZT were analyzed for 3 days. The quantification limit and the detection limit of AZT or succinovlated AZT were determined by reduction of AZT (0.40 µg/ml) or succinoylated AZT (0.41 µg/ml) concentration to a minimum concentration that provided signal-to-noise ratios of 10:1 and 3:1, respectively.

In Vitro Drug Release

Buffer Solutions at pH 5.5 and 7.4

The release of AZT and succinoylated AZT from the dextrin-AZT conjugate was investigated in citrate-phosphate buffer solution at pH 5.5 and PBS at pH 7.4. An aliquot of the dextrin-AZT conjugate (1 ml, 7.23 µmol) was added into 5 ml of preheated buffer $(37\pm0.1^{\circ}C)$ under continuous stirring at 420 rpm using a magnetic stirrer. Paraffin film closures were used to prevent evaporation. Samples (300 µl) were taken at various time intervals and the stavudine internal standard (25 µl, 165 µg/ml) was added. The amounts of AZT and succinovlated AZT released were determined by HPLC analysis.

Human Plasma

An aliquot of the dextrin-AZT conjugate (1 ml, 7.23 μ mol) was added into 5 ml of preheated plasma (37± 0.1°C) under continuous stirring at 420 rpm using a magnetic stirrer. Paraffin film closures were used to prevent evaporation. Samples $(300 \ \mu l)$ were taken at different time intervals. The stavudine internal standard (30 µl, 165 µg/ml) was added, and thoroughly mixed into the collected sample. Trichloroacetic acid (60 μ l, 20% wt/vol) was then added to precipitate plasma proteins. The mixture was vortexed for 30 s and centrifuged at 12,000 rpm for 7 min. The supernatant was analyzed by HPLC







Fig. 3. ¹H-NMR spectra of a AZT in CDCl₃, b succinovlated AZT in CDCl₃, c dextrin in D₂O and d the dextrin–AZT conjugate in D₂O

to determine the amounts of AZT and succinoylated AZT released from the dextrin-AZT conjugate.

Hemolysis Assay

Human red blood cells were separated and washed three times with cold PBS. The red blood cells (RBC) were then diluted in cold PBS to obtain 2% (wt/vol) of RBC suspension. The solutions (100 μ l) of various concentrations of free AZT, the conjugate (calculated equivalent to AZT loading), dextrin, dextran or poly(ethyleneimine) (PEI) in PBS were incubated with RBC suspension (100 μ l) at 37°C for 4 h. The incubated samples were centrifuged at 1,000×g for 10 min to remove the intact RBC. The supernatant (100 μ l) was transferred to 96-well plate. The absorbance was measured at 550 nm using a microtitre plate reader. The percentage of hemolysis was calculated relative to 100% hemolysis obtained from incubation with a 1% vol/vol solution of Triton X-100 (32).

In Vivo Pharmacokinetic Study

Male Sprague Dawley rats weighing 250-300 g were obtained from the National Laboratory Animal Centre (Nakhon Pathom, Thailand). The experimental protocol was approved by the Institutional Animals Ethics Committee of Chulalongkorn University. Three rats were used in each group to investigate the pharmacokinetics of the dextrin-AZT conjugate and AZT following I.V. administration. A freshly prepared solution of either free AZT or the dextrin-AZT conjugate (AZT equivalent dose of 8.46 mg/kg body weight) in sterile normal saline was injected as an I.V. bolus into the tail vein. Blood samples $(150 \,\mu l)$ were taken from the tail vein at different time intervals up to 30 h, and collected in microcentrifuge tubes. The plasma was separated by centrifugation at 12,000 rpm for 10 min, and the resultant supernatants were processed for analysis by HPLC. The plasma half-life $(t_{1/2})$ of AZT was calculated using Eq. 2:

$$t_{1/2} = \frac{0.693}{k_e} \tag{2}$$

where k_e was the elimination rate constant of the terminal elimination phase. The area under the plasma concentrationtime curve (AUC_{0→ α}) and the area under the first moment of the plasma concentration-time curve (AUMC_{0→ α}) were calculated using the trapezoidal rule. The mean residence time (MRT), the apparent distribution volume (V_d) and the systemic clearance (CL) were calculated following Eqs. 3, 4 and 5, respectively:

$$MRT = \frac{AUMC_{0\to\infty}}{AUC_{0\to\infty}},\tag{3}$$

$$V_d = \frac{dose \times AUMC_{0 \to \infty}}{\left(AUC_{0 \to \infty}\right)^2},\tag{4}$$

$$CL = \frac{dose}{(AUC_{0\to\infty})}.$$
 (5)

Statistic Analysis

Statistical significance of differences was assessed using Student's *t* test and analysis of variance (ANOVA) with posthoc Turkey's comparison. The *P*-value of <0.05 was considered statistically significant.

RESULTS AND DISCUSSION

Synthesis and Characterization of the Dextrin-AZT Conjugate

Synthesis of the dextrin–AZT conjugate involved two steps (Fig. 1). Firstly, AZT was succinoylated to introduce a carboxylic functional group by reacting with succinic anhydride in the presence of triethylamine. Then, the succinoylated AZT was conjugated with dextrin by using DCC and HOBt as coupling agents. In brief, AZT reacted with succinic anhydride to form succinoylated AZT, which was purified by solvent extraction and then by flash column chromatography (Sephadex LH-20). The synthetic process provided succinoylated AZT of purity >97%, determined by HPLC. Its FT-IR spectrum (Fig. 2) exhibited a broad band of O-H stretching in the range of 2,700–3,660 cm⁻¹ centered at 3,190 cm⁻¹. The



Fig. 4. MALDI-TOF mass spectra of a dextrin and b the dextrin-AZT conjugate



Fig. 5. HPLC chromatograms of stavudine, AZT and succinoylated AZT in human plasma

azido group $(-N_3)$ appeared at 2,109 cm⁻¹. The carbonyl stretching of the ester of carboxylic acid showed at 1,735 cm⁻¹. The C=O band was a broad band due to the overlap of two esters of the carboxylic acid and of 6 pieposition owing to the incorporation of succinic groups together with carbonyls of -CO-NH-CO- of AZT. The ¹H-NMR in CDCl₃ (Fig. 3) showed the disappearance of the proton of hydroxyl group at 8.55 ppm, the presence of the protons of succinic group at 2.62 ppm and of the carboxylic group at 10.62 ppm. The conjugation of succinovlated AZT and dextrin was carried out in the presence of DCC and HOBt. The structure of the dextrin-AZT conjugate was confirmed by FT-IR and ¹H-NMR. The FT-IR spectrum (Fig. 2) showed the absorption of the $-N_3$ group of succinoylated AZT at 2,113 cm⁻¹. The ester of succinic spacer absorbed at 1,734 cm⁻¹ whereas the amide I and amide II absorptions of succinovlated AZT occurred at 1,648 and 1,568 cm⁻¹, respectively. The remaining unreacted hydroxyl groups of dextrin appeared as a broad band centered at $3,401 \text{ cm}^{-1}$. The CH, CH₂ stretching of dextrin exhibited at 2,930 cm⁻¹ and the absorption of O–CH₂ of dextrin was shown at 1,025 cm⁻¹.

The ¹H-NMR in D_2O of the dextrin-AZT conjugate (Fig. 3) showed a peak at 1.66 ppm due to the methyl protons of succinovlated AZT. The conjugation caused a 0.22 ppm upfield shift of the methyl protons of succinovlated AZT. The signals between 2.31 and 2.53 ppm were from the protons of C2' of sugar ring of succinovlated AZT and those of the succinic spacer. The peak at 5.94 ppm corresponded to the proton of C1' of succinovlated AZT and the peak at 7.28 ppm was due to the proton of C6 on the pyrimidine ring of succinovlated AZT. A small downfield shift of 0.01 ppm for the proton of C1' of succinovlated AZT and an upfield shift of 0.16 ppm for the proton of C6 of succinoylated AZT was observed after conjugation. The broad bands from 2.94 to 5.45 ppm were due to the protons of the dextrin polymer. The MALDI-TOF mass spectrum of the dextrin-AZT conjugate was compared with that of dextrin as shown in Fig. 4. Dextrin had average molecular weight of around 2,264.6 Da. After

conjugation, the dextrin–AZT conjugate had a higher average molecular weight of about 2,980.9 Da indicating the success of conjugation. The absence of free AZT or succinoylated AZT in the dextrin–AZT conjugate was confirmed by HPLC analysis. Drug loading on the polymeric backbone was estimated by UV spectroscopy and found to be 18.9% wt (15.24 mol%). The average AZT content was also confirmed by ¹H-NMR analysis and was in good agreement with that from UV analysis (15.03 mol%).

In Vitro Drug Release

First, the HPLC conditions for quantitation of AZT and succinoylated AZT in plasma were developed and validated. Figure 5 shows the HPLC chromatograms of AZT and



Fig. 6. Release of AZT and succinoylated AZT from the dextrin-AZT conjugate in buffer solutions at pH 5.5 and pH 7.4, at $37\pm0.1^{\circ}$ C. Mean \pm SD, n=3



Fig. 7. Release of AZT and succinoylated AZT from the dextrin– AZT conjugate in human plasma, at 37±0.1°C. Mean±SD, n=3

succinovlated AZT in plasma. Retention times for stavudine internal standard, AZT and succinovlated AZT were 11.9, 20.2 and 26.7 min, respectively. The analytes' peaks were not interfered with endogenous peaks of plasma matrix showing the specificity of the HPLC method. For AZT, the quantitation limit was 0.017 μ g/ml and the detection limit was found to be 0.006 µg/ml. The coefficient of variation for intra-day precision was between 0.5% and 2.5%, and for inter-day precision was between 1.6% and 3.2%. The calibration curve of peak area ratio of AZT/stavudine against the AZT concentration showed good linearity (r^2 of 0.9997). For succinovlated AZT, the quantitation limit was 0.034 µg/ml and the detection limit was 0.008 µg/ml. In this case, the coefficient of variation for intra-day precision and inter-day precision were 0.8-1.7% and 0.9-2.4%, respectively, and the linearity was good (r^2 of 0.9998). The percent recovery of AZT and succinovlated AZT from plasma was found to be 99.3% and 102.1%, respectively.

The drug release profiles of the dextrin-AZT conjugate were investigated in buffer solutions at pH 5.5 (equivalent to the pH of the endosomal compartment) and 7.4 (equivalent to that of extracellular fluids). Theoretically hydrolysis can occur at two sites in the succinic spacer resulting in the release of either free AZT or succinovlated AZT. Figure 6 showed 1.4% of the drug was released from the conjugate at pH 5.5 after 24 h. This release was corresponded to 0.7% AZT and 0.7% succinovlated AZT. At pH 7.4, 41.7% of the drug was released as free drug and succinovlated drug (14.7% and 27.0% respectively). The release profiles of both were almost linear over time with r² values of 0.9948 and 0.9897, respectively. These release profiles followed zero order kinetics, the succinovlated AZT release being greater than that of AZT release (P < .05) indicating that the ester linkage of the succinic spacer bonded to dextrin was more susceptible to hydrolysis than the bond to AZT. The dextrin-AZT conjugate was stable at pH 5.5 but hydrolyzed to release drug at pH 7.4.

In human plasma (Fig. 7), approximately 78% of the bound drug (42.3% AZT and 36.1% succinovlated AZT) was released within 24 h. Initially succinoylated AZT release was greater than for AZT (P < 0.05), however, after 24 h AZT was released from both the dextrin-AZT conjugate and succinoylated AZT. AZT and succinoylated AZT release from the dextrin-AZT conjugate was complete within 48 h and the appearance of AZT was nearly linear (r^2 of 0.9874) with time over 48 h following zero order release. In plasma, the rate of the release of AZT and succinovlated AZT from the conjugate was faster than in buffer at pH 7.4 indicating that the succinic spacer allows the release of drug through both hydrolytic and enzymatic mechanisms. Due to the ester type of the succinic spacer, succinovlated AZT would be cleaved by esterases in the blood resulting in free AZT that exerts its anti-HIV activity. Free succinate (spacer) will be metabolized to fumarate by succinate dehydrogenase (33-35)hence the free spacer would not accumulate and would thus be safe for long-term use of the dextrin-AZT conjugate. In



Fig. 8. Hemolytic effect of **a** dextrin, dextran, poly(ethyleneimine) (PEI) and the dextrin–AZT conjugate and **b** those of the dextrin–AZT conjugate, AZT and combination of AZT and dextrin. Mean \pm SD, n=3



Fig. 9. Free AZT plasma concentrations *versus* time following I.V. administration of the dextrin–AZT conjugate and free AZT to rats. Mean \pm SD, n=3

AIDS compromised patients, the free spacer is metabolized as the same process as in healthy humans.

Hemolysis Study

As the dextrin–AZT conjugate is used for I.V. administration, an *in vitro* hemolysis assay was used as a simple measure of safety determination (36). The degree of hemolysis obtained for the dextrin–AZT conjugate was compared with that of the parent polymer (dextrin), dextran and poly (ethyleneimine) (PEI) as reference controls. Dextran is used as a plasma volume expander in the form of I.V. infusion solutions (37–39). PEI was used as positive control because it has high hemolytic activity. The hemolytic activities of the dextrin–AZT conjugate, dextrin, dextran and PEI are shown in Fig. 8a. The dextrin–AZT conjugate showed a low hemolytic activity that was equivalent to dextrin, dextran (P>0.05) and to AZT (P>0.05) (Fig. 8b). The hemolytic activity of AZT did not increase when it was covalently linked to dextrin or physically mixed with dextrin (P>0.05).

In Vivo Pharmacokinetic Study

The *in vivo* pharmacokinetic study was conducted to compare the pharmacokinetics of the conjugate with free AZT. The plasma concentrations of AZT over time following I.V. administration of the conjugate and free drug are shown in Fig. 9, with the corresponding pharmacokinetic parameters in Table I. After administration of the conjugate, an initial AZT level of 4 µg/ml was observed and after 3 h the AZT concentration was maintained at ~0.10 µg/ml up to 30 h (range, 0.06–0.17 µg/ml), values in the IC₅₀ range (0.03–0.13 µg/ml) for suppression of viral replication (14). Whereas the administration of free AZT showed initial AZT concentration of 24 µg/ml which was six times greater than that obtained from the conjugate but AZT level decreased dramatically to undetectable level after 5 h. This AZT plasma

profile following I.V. administration of the dextrin–AZT conjugate providing more stable drug level may result in a decreased risk of AZT toxicity. With appropriate dose adjustment, the dextrin–AZT conjugate would provide therapeutic levels and it would need less frequent administration.

The pharmacokinetic parameters obtained from administration of the conjugate (Table I) indicated that it improved the pharmacokinetic profile of AZT. The half-life of AZT was increased from 1.3 to 19.3 h (P < 0.05). The mean residence time (MRT) was calculated to be 23.6 h (P < 0.05). The area under the plasma concentration-time curve $(AUC_{0\rightarrow\alpha})$, the area under the first moment of the plasma concentration-time curve $(AUMC_{0\to\alpha})$ and the apparent distribution volume (V_d) obtained following the administration of the dextrin-AZT conjugate were significantly increased (P < 0.05). Moreover, the conjugate exhibited a reduced systemic clearance (CL) (P <(0.05) which could be explained by the higher molecular weight of the conjugate reducing its renal filtration. The in vivo study indicated that the dextrin-AZT conjugate has potential as a polymeric producing sustained release of AZT after I. V. administration. This novel conjugate could be helpful in the treatment of HIV infection providing the required constant drug levels to successfully suppress viral replication.

 Table I. Pharmacokinetic Parameters of AZT Following I.V. Administration of Free AZT and Dextrin–AZT Conjugate, Dose of 8.46 mg/kg in Rats, Mean±SD, n=3

Pharmacokinetic parameters	AZT	Dextrin-AZT conjugate
$k_{\rm e}~({\rm h}^{-1})$	0.527 ± 0.035	0.037 ± 0.008
$t_{1/2}$ (h)	1.32 ± 0.09	19.34 ± 4.93
$AUC_{0 \to \alpha}(\mu g h/ml)$	5.14 ± 0.48	6.09 ± 0.09
$AUMC_{0 \rightarrow \alpha}(\mu g h^2/ml)$	1.78 ± 0.12	142.31 ± 17.70
MRT (h)	0.35 ± 0.02	23.63 ± 3.04
$V_{\rm d}$ (l)	0.16 ± 0.02	9.30 ± 1.25
CL (l/h)	0.47 ± 0.04	0.39 ± 0.01

A Novel Anti-HIV Dextrin–Zidovudine Conjugate

CONCLUSION

The synthesis of a novel dextrin–AZT conjugate has been reported. AZT was covalently attached to the dextrin backbone via ester bonds by succinoylation, and the conjugate formed was stable at pH 5.5 and drug released at pH 7.4, both in buffer and in human plasma *in vitro*. An *in vivo* investigation in rats showed that I.V. administration of the dextrin–AZT conjugate led to a sustained release of AZT over at least 30 h, the pharmacokinetics of AZT were improved and a maintenance plasma level was achieved. The more stable plasma levels obtained using the dextrin– AZT conjugate may also be expected to decrease the fluctuations in drug levels that can lead to toxicity.

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REFERENCES

- R. Yarchoan, R. W. Klecker, K. J. Weinhold *et al.* Administration of 3'-azido-3'-deoxythymidine, an inhibitor of HTLV-III/LAV replication, to patients with AIDS or AIDS-related complex. *Lancet.* 327:575–580 (1986).
- 2. A. M. D'Alessandro, A. C. Rinaldi, G. D'Andrea *et al.* Evidences that zidovudine (AZT) could not be directly responsible for iron overload in AZT-treated patients: an *in vitro* study. *Clin Chim Acta.* **300**:119–130 (2000).
- G. K. McEvoy, J. Miller, E. K. Snow, O. H. Welsh, and K. Litvak (eds.), AHFS Drug information. American Society of Health-System Pharmacists, Bethesda, MD, 2004, pp. 731–745.
- S. Chitnis, D. Mondal, and K. C. Agrawal. Zidovudine (AZT) treatment suppress granulocyte-monocyte colony stimulating factor receptor type alpha (GM-CSFR alpha) gene expression in murine bone marrow cells. *Life Sci.* **71**:967–978 (2002).
- A. S. Fauci. HIV and AIDS: 20 years of science. *Nat Med.* 9:839– 843 (2003).
- S. T. Narishetty, and R. Panchagnula. Transdermal delivery of zidovudine: effect of terpenes and their mechanism of action. J Control Release. 95:367–379 (2004).
- M. D. Lynx, A. T. Bentley, and E. E. McKee. 3'-Azido-3'deoxythymidine (AZT) inhibits thymidine phosphorylation in isolated rat liver mitochondria: a possible mechanism of AZT hepatotoxicity. *Biochem Pharmacol.* **71**:1342–1348 (2006).
- M. L. Newell. Current issues in the prevention of mother-to-child transmission of HIV-1 infection. *Trans R Soc Trop Med Hyg.* 100:1–5 (2006).
- R. W. Klecker Jr., J. M. Collins, R. Yarchoan *et al.* Plasma and cerebrospinal fluid pharmacokinetics of 3'-azido-3'-deoxythymidine: a novel pyrimidine analog with potential application for the treatment of patients with AIDS and related diseases. *Clin Pharmacol Ther.* **41**:407–412 (1987).
- N. S. Thomas, and R. Panchagnula. Transdermal delivery of zidovudine: effect of vehicles on permeation across rat skin and their mechanism of action. *Eur J Pharm Sci.* 18:71–79 (2003).
- D. D. Richman, M. A. Fischl, M. H. Grieco *et al.* The toxicity of azidothymidine (AZT) in the treatment of patients with AIDS and AIDS-related complex. A double-blind, placebo-controlled trial. *N Engl J Med.* **317**:192–197 (1987).

- M. Barry, J. L. Howe, D. J. Back *et al.* Zidovudine pharmacokinetics in zidovudine-induced bone marrow toxicity. *Br J Clin Pharmacol.* 37:7–12 (1994).
- C. Flexner. Antiretroviral agents and treatment of HIV infection. In L. L. Brunton, J. S. Lazo, and K. L. Parker (eds.), Goodman and Gilman's The Pharmacological Basis of Therapeutics, 11th ed., McGraw-Hill, New York, 2006, pp. 1273–1285.
- C. V. Fletcher, T. N. Kakuda, and A. C. Collier. Human immunodeficiency virus infection. In J. T. DiPiro, R. L. Talbert, G. C. Yee, G. R. Matzke, B. G. Wells, and L. M. Posey (eds.), Pharmacotherapy A Pathophysiologic Approach, 4th ed., Appleton and Lange Stamford, Connecticut, 1999, pp. 1937–1938.
- F. G. Hayden. Antimicrobial agents. In J. G. Hardman, L. E. Limbird, P. B. Molinoff, R. W. Ruddon, and A. G. Gilman (eds.), Goodman and Gilman's The Pharmacological Basis of Therapeutics, 9th ed., McGraw-Hill, New York, 1996, pp. 1204–1207.
- C. F. Lacy, L. L. Armstrong, M. P. Goldman, and L. L. Lance. Drug Information Handbook, 15th ed., Lexi-Comp, Hudson, OH, 2007, pp. 1812–1815.
- S. Dumitriu, and M. Dumitriu. Polymeric drug carriers. In S. Dumitriu (ed.), Polymeric Biomaterials, Marcel Dekker, New York, 1994, pp. 474–475.
- K. Hoste, K. D. Winne, and E. Schacht. Polymeric prodrugs. Int J Pharm. 277:119–131 (2000).
- M. Lovrek, B. Zorc, B. Boneschans, and I. Butula. Macromolecular prodrugs. VIII. synthesis of polymer-gemfibrozil conjugates. *Int J Pharm.* 200:59–66 (2000).
- M. Zovko, B. Zorc, M. Lovrek, and B. Boneschans. Macromolecular prodrugs. IX. synthesis of polymer-fenoprofen conjugates. *Int J Pharm.* 228:129–138 (2001).
- 21. R. Duncan. The dawning era of polymer therapeutics. *Nat Rev Drug Discov.* **2**:347–360 (2003).
- S. E. Matthews, C. W. Pouton, and M. D. Threadgill. Macromolecular systems for chemotherapy and magnetic resonance imaging. *Adv Drug Deliv Rev.* 18:219–267 (1996).
- D. Hreczuk-Hirst, L. German, and R. Duncan. Dextrins as carriers for drug targeting: reproducible succinoylation as a means to introduce pendent groups. *J Bioact Compat Polym.* 16:353–365 (2001).
- 24. G. S. diZerega, S. J. Verco, P. Young *et al.* A randomized, controlled pilot study of the safety and efficacy of 4% icodextrin solution in the reduction of adhesions following laparoscopic gynaecological surgery. *Hum Reprod.* 17:1031–1038 (2002).
- S. J. Davies. Exploring new evidence of the clinical benefits of icodextrin solutions. *Nephrol Dial Transplant.* 21(S2):ii47–ii50 (2006).
- C. Sivakama Sundari, B. Raman, and D. Balasubramanian. Artificial chaperoning of insulin, human carbonic anhydrase and hen egg lysozyme using linear dextrin chains-a sweet route to the native state of globular proteins. *FEBS Lett.* 443:215–219 (1999).
- 27. D. S. Davies. Dextrin sulfates as anti HIV-1 agents and composition thereof. US Patent, 5439892 (1969) December 31.
- R. K. Hershline. Antiviral composition. US Patent, 6821958 (2004) November 23.
- C. Flexner, P. A. Barditch-crovo, D. M. Kornhauser *et al.* Pharmacokinetics, toxicity, and activity of intravenous dextran sulfate in human immunodeficiency virus infection. *Antimicrob Agents Chemother.* 35:2544–2550 (1991).
- G. Giammona, G. Cavallaro, G. Fontana, G. Pitarresi, and B. Carlisi. Coupling of the antiviral agent zidovudine to polyaspartamide and *in vitro* drug release studies. *J Control Release*. 54:321–331 (1998).
- International Conference on Harmonization (ICH). ICH topic Q2B validation of analytical procedures: methodology. November 6, 1996.
- B. Carreno-Gomez, and R. Duncan. Evaluation of the biological properties of soluble chitosan and chitosan microspheres. *Int J Pharm.* 148:231–240 (1997).
- P. Y. Bruice. Carbonyl compounds I. In J. Challice, P. F. Corey, C. Trueheart, and K. Schiaparelli (eds.), Organic Chemistry, 2nd ed, Prentice-Hall, Upper Saddle River, NJ, 1998, pp. 679.

- M. S. Olson. Bioenergetics and oxidative metabolism. In T. M. Devlin (ed.), Textbook of Biochemistry with Clinical Correlations, 4th ed., Wiley-Liss, New York, 1997.
- R. H. Garrett and C. M. Grisham. Glycolysis. In J. Vondeling, S. Kiselica, and B. Bonnie (eds.), Principles of Biochemistry with a Human Focus, Brooks/Cole, London, UK, 1997.
- M. Jumaa, F. H. Furkert, and B. W. Muller. A new lipid emulsion formulation with high antimicrobial efficacy using chitosan. *Eur J Pharm Biopharm.* 53:115–123 (2002).
- W. N. van Dijk-Wolthuis, S. K. Y. Tsang, J. J. Kettenes-van den Bosch, and W. E. Hennink. A new class of polymerizable dextrans with hydrolyzable groups: hydroxyethyl methacrylated dextran with and without oligolactate spacer. *Polymer.* 38:6235– 6242 (1997).
- C. Y. Won, and C. C. Chu. Dextran-estrone conjugate: synthesis and *in vitro* release study. *Carbohydr Polym.* 36:327–334 (1998).
- British Pharmacopoeia, Vol. 1, Stationery Office, London, UK, 2002, pp. 567–569.