pH-induced metal-ligand cross-links inspired by mussel yield self-healing polymer networks with near-covalent elastic moduli

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Growing evidence supports a critical role of metal-ligand coordination in many attributes of biological materials including adhesion, self-assembly, toughness, and hardness without mineralization [Rubin DJ, Miserez A, Waite JH (2010) Advances in Insect Physiology: Insect Integument and Color, eds Jérôme C, Stephen JS (Academic Press, London), pp 75–133]. Coordination between Fe and catechol ligands has recently been correlated to the hardness and high extensibility of the cuticle of mussel byssal threads and proposed to endow self-healing properties [Harrington MJ, Masic A, Holten-Andersen N, Waite JH, Fratzl P (2010) Science 328:216–220]. Inspired by the pH jump experienced by proteins during maturation of a mussel byssus secretion, we have developed a simple method to control catechol-Fe³⁺ interpolymer cross-linking via pH. The resonance Raman signature of catechol-Fe³⁺ cross-linked polymer gels at high pH was similar to that from native mussel thread cuticle and the gels displayed elastic moduli (G') that approach covalently cross-linked gels as well as self-healing properties.

biomaterials | catecholate polymer | metal coordination | reversible cross-links | physical gels

Mussel byssal threads are protected against wear by a cuticle, an outer proteinaceous coating, that despite a hardness of ~0.1 GPa, accommodates large cyclic strains in the turbulent intertidal zone (1, 2). During strain, the cuticle suppresses macroscale failure by limiting crack propagation to the microscale (1, 3). It was recently demonstrated that a small amount of Fe (<1 wt%) plays an important role in this mechanism; bonding with the catechol-like amino acid dihydroxy-phenylalanine (dopa) in the cuticle protein, mfp-1 (4–6). Tris- and bis-catechol-Fe³⁺ complexes possess some of the highest known stability constants of metal-ligand chelates (log $K_S \approx 37-40$, where K_S is the equilibrium constant for the complex formation) (7-10) and single molecule tensile tests have demonstrated that the breaking of a metal-dopa bond requires a force only modestly lower than the force required to rupture a covalent bond under identical loading conditions (~0.8 nN vs. ~2 nN, respectively) (11). Harrington et al. proposed a model where the catechol-Fe³⁺ complexes in the cuticle function as sacrificial load-bearing cross-links facilitating extensibility of the material (4). In contrast to covalent bonds, metal-dopa bonds can spontaneously reform after breaking (11) and the model predicts that the damage accumulated in the cuticle could self-heal via reformation of broken catechol-Fe³⁺ complexes (4). Here we describe a strategy for introducing bis- and/or tris-catechol-Fe³⁺ cross-links into a synthetic polymer network and demonstrate that such a network indeed displays high elastic moduli and self-healing properties.

Results

The stoichiometry of catechol-Fe $^{3+}$ complexes (mono-, bis-, or tris-) is controlled by pH via the deprotonation of the catechol

hydroxyls (Fig. 14). The pH required to establish the bis- and tris-complexes is typically reported to be above pH 7 (7, 8, 10), however, the solubility of Fe^{3+} is very low at anything but acidic pH (at pH 7, only 10^{-18} M aqueous Fe^{3+} is present in solution) (12). To our knowledge, this obstacle is one of the primary reasons that no condensed material other than the mussel thread cuticle and adhesive has been established via Fe^{3+} -catechol cross-links above pH 7 (5, 7, 9, 13, 14). By mimicking the mussel's own process for byssus formation, we have overcome this difficulty and devised an original method with which to form catechol-Fe³⁺ polymer cross-links at basic pH that avoids Fe^{3+} precipitation.

Byssal threads self-assemble in the ventral groove of the mussel foot upon secretion of preassembled thread materials from intracellular granules of byssal gland cells (15). The byssus secretion has recently been proposed to be acidic (pH ~5-6) (16) and will be more fully described elsewhere. We propose that Fe³⁺ is prebound in mono-dopa-Fe³⁺ complexes by mfp-1 in secretory granules at pH \leq 5. Upon release into seawater (pH ~ 8), the significant pH jump would cause nascent thread cuticle material to undergo a spontaneous cross-linking via bis- and/or tris-dopa-Fe³⁺ complexes (see Fig. 1*B* for schematic). To test this mechanism of pH-controlled cross-linking we used a simple dopa-modified polyethylene glycol polymer (PEG-dopa₄, Fig. 2A). We first verified the stoichiometric transitions of the catechol-Fe³⁺ complexes expected with increasing pH by reacting dilute PEG-dopa₄ with FeCl₃ in a dopa: Fe molar ratio of 3:1 (Fig. S1). The initially green solution turned blue and finally red as the catechol-Fe³⁺ stoichiometry changed from mono- to bis- to tris-, respectively. Identical shifts in absorbance have been reported elsewhere (17). The relative fractions of the three coordination states, extracted from the absorbance data (see Methods for details), show that the monospecies dominate at pH < 5.6, bisat 5.6 < pH < 9.1, and tris- at pH > 9.1 (Fig. 2*B*). We next tested the effect of catechol-Fe $^{3+}$ cross-linking on concentrated polymer networks (dopa:Fe 3:1) at pH~5 (proposed pH of secretory granules), $pH \sim 8$ (pH of seawater), and $pH \sim 12$ (complete tris-catechol-Fe3+ cross-linking). Employing our mussel-inspired method of prebinding Fe³⁺ in mono-catechol-Fe³⁺ complexes at acidic pH successfully prevents ferric hydroxide precipitation

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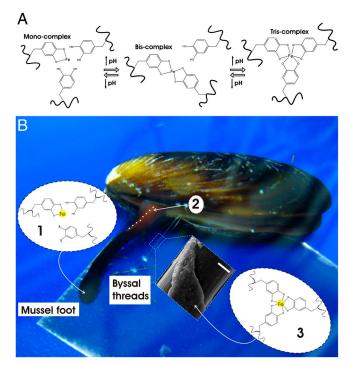


Fig. 1. Mussel-inspired Dopa-Fe³⁺ cross-linking. (*A*) The pH-dependent stoichiometry of Fe³⁺-catechol complexes. (*B*) Schematic of proposed crosslinking mechanism of byssal thread cuticle: (*i*) Production and storage of mfp-1 and Fe³⁺ in specialized cells of the epithelium lining the ventral groove of the mussel foot. Low pH (\leq 5) ensures mono-catechol-Fe³⁺ complexes (no cross-linking), (*ii*) Secretion and self-assembly of cuticle with whole mussel thread in the ventral groove (outline of part of ventral groove indicated with dashed white line), (*iii*) Seawater exposure (pH ~8) of nascent byssal thread drives immediate cuticle cross-linking via bis- and/or tris-catechol-Fe³⁺ complexes (insert shows scanning electron micrograph of mussel thread with partial cuticle on top of fibrous core) (Scale bar, 20 µm).

when raising pH to initiate cross-linking. The concentrated polymer-FeCl₃ mixture remained a green/blue fluid upon raising pH to ~5, whereas raising pH to ~8 resulted in the instant formation of a sticky purple gel. At pH ~ 12 a red elastomeric gel immediately formed (Fig. 2C and Fig. S2 A-C, G, I, and Movie S1). UV-Vis absorbance spectroscopy confirmed the dominance of mono-, bis-, and tris-catechol- Fe^{3+} complexes, in the pH ~ 5, ~8, and ~12 adjusted polymer networks, respectively (Fig. S1). Raman microspectroscopy performed with a near-infrared (785 nm) laser furthermore demonstrated resonance Raman spectra characteristic of Fe³⁺-catechol coordination in the polymer networks after FeCl₃ was added (Fig. 2D). Clear spectral differences exist between samples, particularly in the Raman band originating specifically from the chelation of the Fe^{3+} ion by the oxygen atoms of the catechol (470-670 cm⁻¹). This band consists of three major peaks, which transform significantly with changing pH. The peaks at \sim 590 cm⁻¹ and \sim 633 cm⁻¹ are assigned to the interaction between the Fe³⁺ ion and the C₃ and C₄ oxygens of the catechol, respectively, while the peak at 528 cm⁻¹ is assigned to charge transfer (CT) interactions of the bidentate chelate (see Fig. 1A) (18). The area of the CT peak increases relative to the other two peaks upon increasing pH from about 6% at pH ~ 5 to ~30% at pH ~ 8 and almost 40% at pH ~ 12. This peak progression suggests an increase in bidentate complexation with increasing pH consistent with the transition from mono- to tris-coordinated Fe³⁺ species. Moreover, the resonance signals from the tris-catechol- Fe^{3+} cross-linked gels at pH ~ 12 and reconstituted Fe^{3+} mfp-1 complexes (7) were found to be remarkably similar to the native thread cuticle (Table S1 and Fig. 2D) (4).

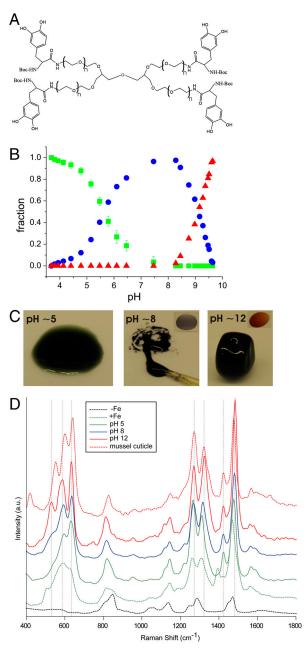


Fig. 2. PEG-dopa₄-Fe³⁺ crosslinking. (A) Dopa-modified polyethylene glycol (PEG-dopa₄, 10 kDa PEG core). (B) Relative fractions of mono- (green), bis- (blue), and tris-catechol-Fe³⁺ (red) complexes in solutions of PEG-dopa₄ with FeCl₃ at a dopa:Fe molar ratio of 3:1 as a function of pH. (C) Physical state and color of PEG-dopa₄ gels in mono- (green/blue), bis- (purple), and tris-catechol-Fe³⁺ (red) complexation (dopa:Fe 3:1). Insets highlight color of bis- and tris-catechol-Fe³⁺ cross-linked gels. (D) Resonance Raman spectroscopy of the same samples as in (C). Spectra of PEG-dopa₄ without (dashed black) and with (dashed green) FeCl₃ (unadjusted pH ~3–4) are shown for comparison. Additionally, the spectrum from the native mussel thread cuticle is included (dashed red). For each spectra N = 3.

In agreement with their lack of cross-linking, concentrated polymer-FeCl₃ mixtures at pH ~ 5 displayed a viscous response in dynamic oscillatory rheology, whereas the bis- and tris-catechol-Fe³⁺ cross-linked gels at pH ~ 8 and pH ~ 12, respectively, behaved increasingly elastically (elastic modulus G' > viscous modulus G'') (Fig. 3*A*). For comparison, a covalently cross-linked polymer gel was prepared using NaIO₄-induced oxidation of PEG-dopa₄ (19) (Fig. S2 *D*–*H*). When a tris-catechol-Fe³⁺ crosslinked gel and a covalent gel were exposed to a concentrated

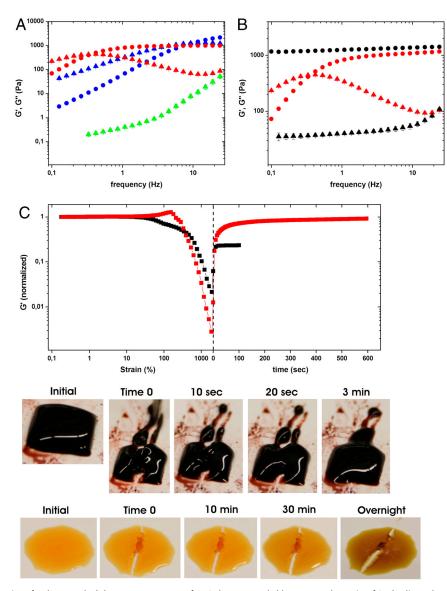


Fig. 3. Mechanical properties of polymer gels. (*A*) Frequency sweep of PEG-dopa₄ Fe-gels (dopa: Fe molar ratio of 3:1) adjusted to pH ~5 (green), pH ~8 (blue), and pH ~12 (red), storage modulus (G', circles) and loss modulus (G", triangles). (*B*) Comparison of gels cross-linked with tris-catechol-Fe³⁺ complexes (red) or with covalent bonds (black) (G' and G", circles and triangles, respectively). (*C*) Recovery of stiffness and cohesiveness after failure induced by shear strain or simple tearing with the tip of a set of tweezers of tris-catechol-Fe³⁺ gels (red curve and top row of images) and covalent gels (black curve and bottom row of images). Gels were shear failed under increasing oscillatory strain immediately followed by recovery under 1% strain (switch-over indicated by dashed line) while monitoring the storage modulus (G' is normalized to values from linear regime, <60% strain, to allow easier comparison). For each data point (mean) N = 4 (except for in Fig. 3*C* where N = 2).

solution of the Fe³⁺ chelating agent EDTA at pH 4.7, only the former dissolved (Fig. S3). This result supports the notion that the redox activity of Fe³⁺ does not lead to significant covalent cross-linking via oxidation of catechol within the time frame of our experiments (<4 h) as has been reported in other systems (9), however, the potential introduction of covalent cross-linking from Fe³⁺ redox activity is under current investigation. The triscatechol-Fe³⁺ cross-linked gel was observed to dissipate > 10-fold more energy (G") than the covalent gel at low strain rates, even though the elastic moduli (G') were similar at high strain rates (Fig. 3*B*). Finally, following failure induced by shear strain or simple tearing, tris-catechol-Fe³⁺ cross-linked gels recovered G' and cohesiveness within minutes whereas the covalently cross-linked gels did not (Fig. 3*C*).

Discussion

We demonstrate that load-bearing catecholato- Fe^{3+} cross-links can be established in bulk materials by mimicking the proposed

cross-linking strategy that the mussel employs during byssus secretion. By following this strategy the mechanical properties of catechol-Fe³⁺ polymer networks can be easily controlled because the networks behave according to the average lifetime of their catechol-Fe³⁺ cross-links set by final pH (20). The pH-induced shifts of the frequency of maximum viscous dissipation (f_{max}) observed in shear rheometry demonstrates this effect (21). As the pH of cross-linking increases from ~8 to ~12, f_{max} shifts from \approx 14.3 Hz (mean, SE 0.5, N = 4) to \approx 0.39 Hz (mean, SE 0.01, N = 6) in agreement with a decrease in cross-link dissociation rate (see Fig. 3A). Our data suggest average relaxation times τ (1/f_{max}) of $\tau \approx 0.070$ s and $\tau \approx 2.56$ s, respectively, for bisand tris-catechol-Fe³⁺ cross-linked networks. The near covalent stiffness (G') of tris-catechol-Fe³⁺ cross-linked networks at high strain rates (see Fig. 3B) supports the hypothesis that catecholato-Fe³⁺ coordinate bonds can provide significant strength to bulk materials despite their transient nature, given that the pH is high enough to ensure cross-link stability on relevant time scales.

Additionally, the tris-catechol-Fe³⁺ cross-linked gels reestablish their stiffness and cohesiveness within minutes after failure (see Fig. 3*C*) likely through restoration of broken catecholato-Fe³⁺ cross-links analogous to what has been observed in other types of reversible polymer networks with weaker noncovalent cross-links such as ionic and hydrogen bonds (22, 23). The effects of polymer size, cross-link density, and Fe: dopa ratio on the relaxation and self-healing time of catecholato-Fe³⁺ cross-linked polymer networks are currently under investigation.

Although the relevance of our findings to byssus formation remains tentative at this time, to a first approximation, we have measured the effect of the proposed pH jump from secretory granules to seawater on catecholato-Fe³⁺ cross-linked polymer networks. The overall similarity of the resonance signals from tris-catechol-Fe³⁺ cross-linked gels and reconstituted Fe³⁺ mfp-1with native mussel thread cuticle (see Table S1 and Fig. 2D) supports that tris-dopa-Fe³⁺ complexes cross-link mfp-1 in the natural coating. However, the Raman signature of the mussel thread cuticle is more similar to gels cross-linked at pH ~ 12 than at the pH of seawater and small differences were found between tris-catechol-Fe³⁺ cross-linked gels and cuticle. These disparities likely arise from differences in the microenvironment and conformation between mfp-1 protein in the native thread cuticle and our in vitro polymer scaffolds.

The viscoelastic properties that arise from catecholato- Fe^{3+} cross-links in polymeric networks could be advantageous to the mussel in the following ways. A concentrated secretion of mfp-1, weakly cross-linked with low levels of bis-dopa- Fe^{3+} complexes initially, could provide ideal properties for coating deposition as a viscous fluid similar to what has been proposed for the underwater sandcastle glue of *Phragmatopoma californica* (24). Once fully exposed to ocean pH, during periods of strong wave action with fast flows, the high stiffness of a tris-dopa- Fe^{3+} cross-linked mfp-1 scaffold, combined with its capacity to yield before covalent failure of the protein backbone, would offer ideal protection of the mussel thread. Periods of low wave action could subsequently allow the microdamage developed in the cuticle to self-heal.

These adaptive properties of the thread coating would not only have value to mussels but to engineers as well and in contrast to the mussel adhesive proteins, PEG-dopa polymers are not limited to iron as the cross-linking metal. Dopa has high affinities for other metals, and we have preliminary data illustrating that titanium ions result in the formation of gels with different viscoelastic properties (Fig. S4). The distinct chemical properties of the coordination complexes between PEG-dopa and different metals, including possible covalent cross-linking induced by varying metal redox activities, expand the range of accessible synthetic material properties and are currently under investigation. Furthermore, other metal-coordinating ligands than catechols, could be envisaged to decorate PEG or other types of water soluble polymer backbones with desirable properties and applied in pH-controlled polymer cross-linking following our protocol. In general, cross-linking of polymer networks by metal-ligand coordination has manifold advantages: (i) Relative to covalent cross-linking, metal-ligand coordination offers the promise of materials with comparable strength plus intrinsic self-healing. (ii) Vis-à-vis other reversibly cross-linked polymer networks based on electrostatic, H-bond, or hydrophobic interactions (25–27), cross-linking based on multiple ligand-metal complexes such as metal-catecholates offers near covalent stabilities with noncovalent reformation rates and a range of possible cross-link modes from zero to three per metal ion. (iii) While the metalligand-complex theme can also be utilized to cross-link polymers in organic solvents (28) its incorporation into polymers in aqueous solvents under ambient conditions by simply increasing pH as presented here, provides a unique promising platform for environmental and physiological applications. (iv) Finally, in our initial polymer system, the pH-tunable cross-link kinetics offer easy control of viscoelastic properties over four orders of magnitude in modulus, from a low viscosity fluid to a stable self-healing gel. Adhesives and coatings based on PEG-dopa are already recognized to impart substantial advantages for applications in dry and wet environments (29, 30). Our findings significantly amplify the scope of these.

Methods

Synthesis of $\ensuremath{\text{PEG-(N-Boc-dopa)}_4}\xspace.$ Polymer was synthesized as described in Lee et al. (19). Briefly, 4-arm-PEG-amine [PEG-(NH₂)₄, $M_w = 10,000$] was purchased from SunBio, Inc. PEG-(NH₂)₄ (6.0 g, 0.60 mmol) was reacted with N-Boc (butoxycarbonyl)-L-DOPA dicyclohexylammonium salt (4.8 mmol), HOBt (1-Hydroxybenzotriazole) (8.0 mmol), and Et₃N (8.0 mmol) in 60 mL of a 50:50 mixture of dichloromethane and dimethylformamide. HBTU [2-(1h-benzotriazol-1-yl)-1,1,3,3-tetramethyluronium hexafluorophosphate] (4.8 mmol) in 30 mL of dichloromethane was then added, and the coupling reaction was carried out under argon at room temperature for 1 h. The solution was successively washed with saturated sodium chloride solution, 5% NaHCO₃, diluted HCl solution, and distilled water. The crude product was concentrated under reduced pressure and purified by column chromatography on Sephadex LH-20 with methanol as the mobile phase. The product was further purified by precipitation in cold methanol three times, dried in a vacuum at room temperature, and stored under nitrogen at -20 °C. Gel permeation chromatography-multiple-angle laser light scattering revealed an increase in polymer molecular weight of ~1,400 compared to the starting material in agreement with addition of four butoxycarbonyldopa groups.

Fe³⁺-Catechol Cross-Linked Gels. The above described PEG-(N-Boc-dopa)₄ was used for all gel experiments. Freeze-dried aliquots of the polymer stored under Argon or N_2 at -20 °C, were equilibrated to room temperature for 1 h before opening sample vial to prevent water condensation on the sample. A typical 400 μL Fe^{3+}-catechol cross-linked gel was made as follows: 1) 200 µL of polymer solution was prepared by dissolving 40 mg polymer in unbuffered Milli-Q water to a starting concentration of 200 mg/mL (corresponds to a dopa concentration of 80 mM). 2) The polymer solution was mixed with 1/6 final volume (66.7 $\mu L)$ of 80 mM (13 mg/mL) FeCla (Sigma). A green color developed immediately upon mixing (see Fig. S2A). 3) The gel was established by adding 2/6 final volume (133.3 µL) of NaOH (Sigma) at a concentration adjusted to induce the desired final pH of the gel. This resulted in instant gelation and color development according to gel pH (see Fig. S2B). 4) The gel was physically mixed until a homogenous color and physical state were established (~60 s). A short movie that illustrates the gel formation is available (see Movie S1). Samples were tested in rheology immediately after mixing, except for gels compared to covalent gels which were then sealed in airtight containers to prevent dehydration (~6 h cure time). The final concentration of PEG-(N-Boc-dopa)₄ in all gels was thereby 100 mg/mL (10 wt%) with a final molar ratio of dopa to $FeCl_3$ of 40 to 13.3 mM (3:1). This corresponds to 0.74 mg/mL (0.074 wt%) of Fe. We established samples at a final $pH \sim 5$ (predominantly mono-catecholato-Fe³⁺ complexes at the proposed pH of secretory granules), pH ~ 8 (predominantly bis-catecholato-Fe $^{3+}$ cross-links at the pH of seawater), and pH \sim 12 (pure triscatecholato-Fe³⁺ cross-links). The pH of gels was measured using a pH-meter with a flat surface electrode designed for solids, semisolids, and liquids (FieldScout SoilStik pH Meter, Spectrum Technologies).

Ti-Cross-Linked Gels. The above protocol for formation of Fe^{3+} -catechol cross-linked PEG-dopa₄ gels was followed substituting FeCl₃ with TiCl₃ (Sigma) using a total of 6 M equivalents of NaOH when inducing the cross-linking.

Covalently Cross-Linked Gels. These gels were established by mixing 200 mg/mL polymer solution with an equal volume of 40 mM (8.6 mg/mL) NalO₄ (dopa: IO_4^- molar ratio of 2:1) (Sigma) which resulted in immediate orange color development and slow gelation (see Fig. S2 *D* and *E*). The covalent gels needed to be precast before they cured due to the elastic nature of the final gel material. Immediately after casting, the samples were sealed in airtight containers until rheology testing (~6 h cure time), except for tests of cross-linking rate where an enclosed test cell served to avoid sample dehydration.

Rheology of Gels. The mechanical properties of the hydrogels were tested using a rheometer (Anton Paar) with parallel plate geometry (25 mm or 50 mm diameter rotating top plate). All tests (except for tests of the rate

of cross-linking) were done immediately after transferring the gel sample onto the sample stage. Oscillatory shear testing of gels as a function of frequency was performed at constant 10 mrad strain (~20% strain, linear viscoelastic regime $0-\sim 60\%$ strain) while measuring storage modulus (G') and loss modulus (G"). Recovery tests were performed by straining each gel to failure under increasing oscillations to 1,000 mrad immediately followed by linear conditions (1% strain, 1 Hz) while monitoring the recovery of the storage modulus (G'). For both types of gels, G' was normalized to values in the linear regime to allow easier comparison. Water loss during testing was negligible due to typical gap distances between parallel plates of ~0.4 mm and typical test time of <30 min. During longer measurements of the rates of cross-linking, the tests were performed in an enclosed cell as a precaution to avoid sample dehydration. All tests were performed at 20 °C. Data points that represents measurements of G' of the pH 5 sample have been removed from the plot in Fig. 3A due to excessive interference from equipment resonance on samples with such low elasticity.

Absorbance Spectrophotometry. The dopa-Fe³⁺ cross-linking stoichiometry and the dopa oxidation were monitored on a UV-visible light spectrophotometer (Perkin Elmer) using a quartz cuvette with a path length of 1 cm. Spectral changes of solutions of $1\ mg/mL\ PEG-dopa_4$ (0.4 $mM_{dopa})$ with 22 µg/mL (0.13 mM) FeCl₃ (dopa: Fe molar ratio of 3:1) were followed while increasing pH with 1 M NaOH up to a final pH ~ 10. The absorbance of 4 mg/mL PEG-dopa₄ (1.6 mM_{dopa}) with 4.3 mg/mL (0.8 mM) NalO₄ (dopa: IO_{4}^{-} molar ratio of 2:1) was monitored immediately following mixing. Furthermore, the absorbance of 4 mg/mL PEG-dopa₄ with 88 µg/mL FeCl₃ (dopa:Fe 3:1) before and after increasing pH from ~3 to ~9 was recorded for comparison with the NaIO₄ induced spectral changes. Absorbance of gels was measured holding the gel between two cover slips and placing them directly in the light path of the spectrophotometer.

To extract the relative abundance of the three dopa-Fe³⁺ cross-linking species, the UV/VIS absorbance data from Fig. S1 were fitted to peak functions in an iterative manner to obtain spectra of the three species that could be used to fit all spectra. For quantification, only the peaks above 400 nm were used because the data below this range were too severely affected by overlap; the main absorption above 400 nm of the monospecies was found to be a doublet at 406 and 759 nm, the dimer had a peak at 575 nm while the trimer had a peak at 492 nm. These values agree with spectra reported in the literature for similar species (9, 10, 31). The areas of the peaks were then normalized to the maximum value for each peak. No constraints on the sum

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of the fractions were imposed during the fitting procedure. Gratifyingly, the largest deviation from unity was 3.4 estimated standard deviations (esd) with an average of 1.6 esd indicating that the fits successfully distributed the intensity into the respective contributions. The data shown in Fig. 2B have been normalized so that the sum of the mole fractions is equal to one.

Resonance Raman Spectroscopy. For Raman spectroscopic studies, a continuous laser beam was focused on the samples through a confocal Raman microscope (CRM200, WITec) equipped with a piezo-scanner (P-500, Physik Instrumente). The diode-pumped 785 nm near infrared laser excitation (Toptica Photonics AG) was used in combination with a 20× microscope objective (Nikon, NA = 0.4). The spectra were acquired using an air-cooled CCD (DU401A-DR-DD, Andor) behind a grating (300 g mm⁻¹) spectrograph (Acton, Princeton Instruments Inc.) with a spectral resolution of 6 cm⁻¹. Because the samples were sensitive to burning by the laser beam, a laser power of between 10-20 mW, combined with a short integration time of 0.2 s was used for all measurements. The ScanCtrlSpectroscopyPlus software (version 1.38, Witec) was used for measurement setup and spectral processing. Each collected spectra consisted of 60 accumulations of a 0.2 s integration time. For each sample, three spectra were collected from different regions and averaged. Averaged spectra were smoothed with a Savitzky-Golay smoothing filter, and a second order polynomial background was subtracted from the smoothed spectra (4, 7, 32, 33).

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