

# Nanoparticle-mediated drug delivery to tumor vasculature suppresses metastasis

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Integrin  $\alpha v\beta 3$  is found on a subset of tumor blood vessels where it is associated with angiogenesis and malignant tumor growth. We designed an  $\alpha v\beta 3$ -targeted nanoparticle (NP) encapsulating the cytotoxic drug doxorubicin (Dox) for targeted drug delivery to the  $\alpha v\beta 3$ -expressing tumor vasculature. We observed real-time targeting of this NP to tumor vessels and noted selective apoptosis in regions of the  $\alpha v\beta 3$ -expressing tumor vasculature. In clinically relevant pancreatic and renal cell orthotopic models of spontaneous metastasis, targeted delivery of Dox produced an antimetastatic effect. In fact,  $\alpha v\beta 3$ -mediated delivery of this drug to the tumor vasculature resulted in a 15-fold increase in antimetastatic activity without producing drug-associated weight loss as observed with systemic administration of the free drug. These findings reveal that NP-based delivery of cytotoxic drugs to the  $\alpha v\beta 3$ -positive tumor vasculature represents an approach for treating metastatic disease.

antiangiogenic | intravital microscopy | pancreatic cancer | renal cell carcinoma | liposome

Angiogenesis contributes to tumor malignancy and is linked to a wide variety of inflammatory and ischemic diseases. Integrin  $\alpha v\beta 3$ , an internalization receptor for a number of viruses (1, 2), was shown to be preferentially expressed on the angiogenic endothelium in malignant or diseased tissues (3, 4). These characteristics of integrin  $\alpha v\beta 3$  make it an attractive targeting molecule for molecular imaging and delivery of therapeutics for cancer. Previous studies have shown that  $\alpha v\beta 3$ -targeted nanoparticles (NPs) coupled to contrast agents can readily image the tumor vasculature revealing “hot spots” of angiogenesis within the tumor (5, 6). Therapeutic studies using the  $\alpha v$  integrin-targeting peptide, RGD-4C, demonstrated that this peptide effectively targeted doxorubicin (Dox) to the tumor neovasculature and enhanced efficacy in human breast cancer xenografts in mice (7). In another study, an  $\alpha v\beta 3$ -targeted NP delivering a suicide gene to angiogenic blood vessels was capable of producing an anticancer response (8). Although integrin  $\alpha v\beta 3$  is a marker of angiogenic endothelium, histological analysis of breast cancer biopsy tissue revealed that  $\alpha v\beta 3$  was a primary marker of blood vessels within the most malignant tumors (4). In fact, a strong correlation was established between the percent of  $\alpha v\beta 3$ -positive vessels within the tumor and disease progression (9).

Here, we report the design and characterization of an  $\alpha v\beta 3$ -targeted NP capable of delivering various pharmacological agents to the  $\alpha v\beta 3$ -expressing tumor vasculature. Evidence is provided that an  $\alpha v\beta 3$ -targeted NP carrying the cytotoxic drug Dox is capable of controlling the metastatic behavior of pancreatic and renal cell cancer in mice. Importantly, targeted delivery of Dox to the tumor vasculature provided a 15-fold increase in the efficacy of the drug while producing few, if any, side effects.

## Results

**Design of NPs Targeted to Angiogenic Endothelium.** A schematic representation of the targeted NP (RGD-NP) (Fig. 1A), which is composed of distearoylphosphatidylcholine (DSPC), chole-

sterol, dioleoylphosphatidylethanolamine (DOPE), distearoylphosphatidylethanolamine (DSPE)-mPEG2000, and DSPE-cyclic RGDfK. After dehydration/rehydration and sonication, the NPs were stepwise extruded down through a minimum pore size of 100 nm. Dynamic light scattering demonstrated that the NPs had a mean hydrodynamic diameter of 105 nm and a zeta potential close to neutrality [supporting information (SI) Table S1]. A 6-(((4,4-difluoro-5-(2-thienyl)-4-bora-3a,4a-diazas-indacene-3-yl)styryloxy)acetyl) aminohexanoic acid, succinimidyl ester (BODIPY) 630/650 fluorophore was conjugated to DOPE, and this fluorescent lipid was incorporated into the particle at low concentration for imaging both *in vitro* and *in vivo* targeting. To address the specificity of the NPs for integrin  $\alpha v\beta 3$ , we performed binding studies on human umbilical vein endothelial cells (HUVECs) that express high levels of this integrin (Fig. 1B). HUVECs were pretreated with a 20-fold molar excess of either cRGDfK (targeting peptide) or cRADfK (control peptide), and the RGD-NPs were subsequently incubated with the cells. RGD-NPs bound and internalized within 20 min in the presence of the cRADfK peptide as expected, whereas the soluble cRGDfK peptide completely inhibited the binding of the RGD-NPs (Fig. 1B).

**In Vivo Targeting of the RGD-NPs.** After establishing targeting *in vitro*, the RGD-NPs were tested for targeting to the tumor vasculature. M21L-GFP mouse melanoma cells (integrin  $\alpha v\beta 3$  negative) were implanted in dorsal skin-fold window chambers and allowed to grow and become vascularized for 7 days. We then injected RGD-NPs (targeted) or RAD-NPs (nontargeted) and imaged both the tumor (GFP) and NPs (BODIPY) by confocal microscopy. RGD-NPs targeted the newly forming tips of the tumor neovasculature associated with the tumor margin within 2 h and reached maximum binding  $\approx 5$  h after i.v. injection, whereas the corresponding RAD-NP did not accumulate in the tumor neovasculature at all time points examined (Fig. 1C).

**RGD-Dox-NPs Are Antiangiogenic.** To study the antiangiogenic effect of the targeted NP, mice containing s.c. Matrigel plugs loaded with basic fibroblast growth factor (bFGF) were i.v. injected with NPs containing Dox. Angiogenesis was measured after 7 days by labeling the vasculature with fluorescein-labeled *Griffonia simplicifolia* lectin (10). It is important to note that this is a model of normal angiogenesis induced by a proangiogenic factor and not a model of tumor angiogenesis. Animals treated with RGD-Dox-NPs (1 mg/kg total Dox) demonstrated vascular

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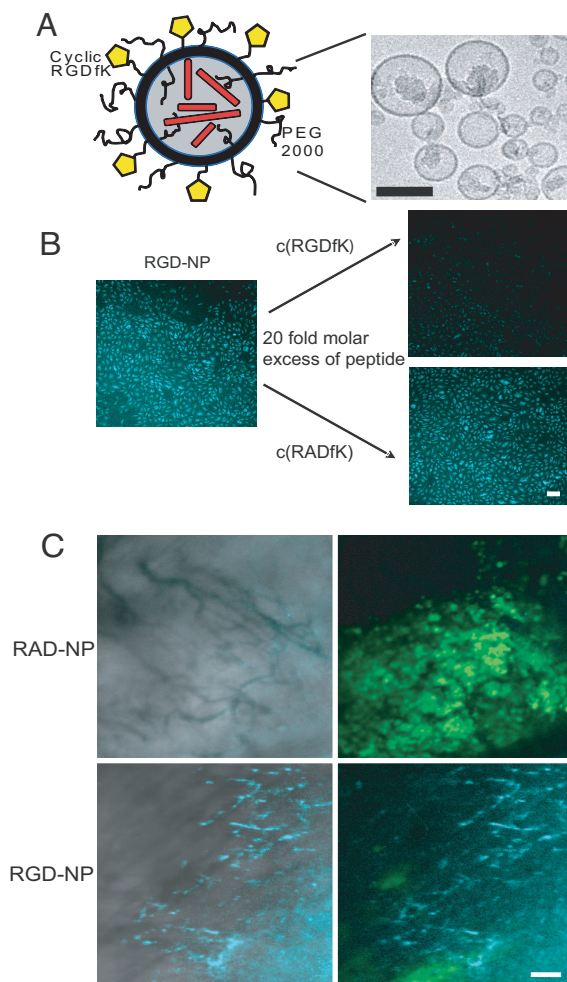
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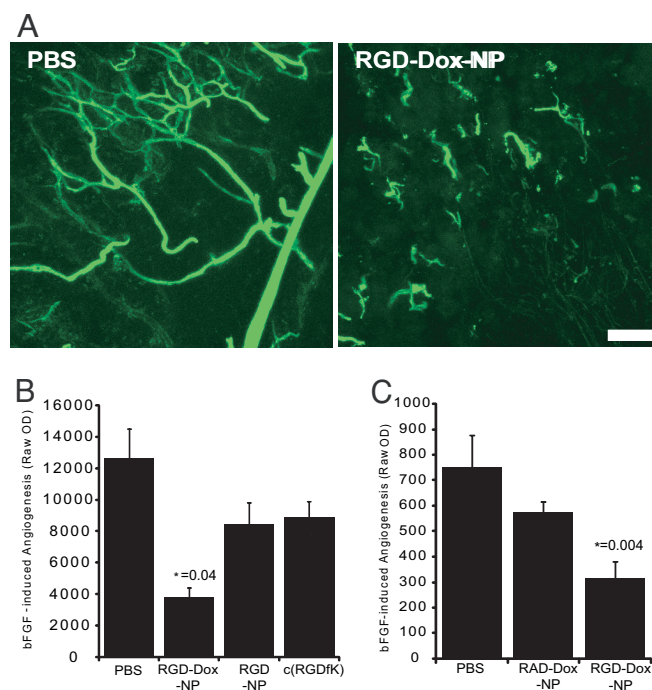
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**Fig. 1.** *In vitro* and *in vivo*  $\alpha v \beta 3$  targeting of RGD-NP. (A) Schematic representation and transmission EM of Dox-loaded RGD-NP. (B) Competition assay for *in vitro*  $\alpha v \beta 3$  targeting of RGD-NP in endothelial cells. HUVECs were pretreated for 5 min with a 20-fold molar excess of either cRGDfK or cRADfK to test for inhibition of NP binding. Subsequently, the cells were incubated with the RGD-NPs for 20 min, and binding was studied by scanning confocal microscopy for the BODIPY 630/650 dye. (C) *In vivo* integrin  $\alpha v \beta 3$  targeting of RGD-NPs within the tumor neovasculature was studied by intravital microscopy with the dorsal skin-fold window chamber. M21L melanomas ( $\alpha v \beta 3$  negative) were allowed to vascularize for 7 days, and mice were i.v.-injected with 200 nmol of either RGD-NP or RAD-NP containing BODIPY 630/650. NPs were imaged by confocal scanning microscopy at 5-h postinjection. GFP-labeled M21L melanomas are shown in green, and NPs are in blue. (Scale bars: A, 100 nm; B and C, 100  $\mu$ m.)

pruning when compared with the normal vascular structure and branching of animals treated with PBS (Fig. 2A) and inhibited angiogenesis by  $\approx 70\%$  (Fig. 2B). Although the cyclic RGDfK peptide has been previously shown to be an integrin  $\alpha v \beta 3$  antagonist (11, 12), minimal response was observed when testing RGD-NP without Dox or cyclic peptide alone (Fig. 2B). Also, RAD-Dox-NPs demonstrated only a marginal reduction (24%) in neovascularization relative to control animals (Fig. 2C). These findings reveal that integrin  $\alpha v \beta 3$  targeting of Dox containing NPs produces a strong antiangiogenic effect.

**Comparison of RGD-Dox-NP Efficacy on Primary vs. Metastatic Sites in Pancreatic Carcinoma.** We next evaluated the targeting and efficacy of the RGD-Dox-NPs in a syngeneic murine orthotopic tumor model of pancreatic carcinoma. R40P murine



**Fig. 2.** Vascular disruption in the mouse Matrigel model with  $\alpha v \beta 3$ -targeted RGD-Dox-NP. Mice were injected s.c. on the flank with Matrigel containing 400 ng of human recombinant bFGF. NPs containing 1 mg/kg of Dox were i.v.-injected on days 1, 3, and 5. (A) After the treatment, mice were i.v.-injected with fluorescein-labeled *G. simplicifolia* lectin and the plugs were removed and imaged by scanning confocal microscopy. (B and C) To quantify angiogenesis, the matrigel plugs were removed and the fluorescent-lectin content was quantified with a fluorimeter. \*,  $P < 0.05$  for RGD-Dox-NP vs. PBS. (Scale bar: 100  $\mu$ m.)

pancreatic cancer cells derived from a spontaneous murine pancreatic tumor (13) were injected into the tail of the pancreas. After 11 days of tumor growth, we injected fluorescent RGD-NPs i.v. and observed accumulation of the RGD-NPs in the pancreatic tumor vasculature but not in the vasculature of the adjacent normal pancreatic tissue (Fig. 3A). Additionally, tissues that manifest a filtration function exhibit detectable concentrations of NPs, albeit at significantly lower fluorescence intensities than the tumor tissue. Specifically, we observed minimal accumulation of the RGD-NPs in the kidney, liver, and lung but found no accumulation in the brain, heart, or spleen (Fig. 3A and B).

For efficacy studies, mice implanted with orthotopic pancreatic tumors were treated on days 5, 7, and 9, and the effects of the RGD-Dox-NPs were observed on day 11. The primary pancreatic tumors were sectioned and analyzed by immunohistochemistry. The serial sections of primary tumors treated with RGD-Dox-NPs were stained with hematoxylin and eosin and analyzed for total blood vessels,  $\beta 3$ -positive blood vessels, and apoptosis (TUNEL stain) (Fig. 3C). For tumors treated with RGD-Dox-NPs at 1 mg/kg (as in Fig. 3D), we observed apoptosis in angiogenic hot spots that corresponded to the  $\beta 3$  positive blood vessels associated with the tumor margin (Fig. 3C). No apoptosis was observed in areas corresponding to  $\beta 3$ -negative vessels. Additionally, no apoptosis was observed in tumors treated with the RAD-Dox-NPs, even when  $\beta 3$ -expressing blood vessels were present (data not shown).

Orthotopically implanted R40P cells typically form metastatic lesions in the hepatic hilar lymph node, which is important because regional lymph node metastasis is an important predictor for survival of pancreatic adenocarcinoma patients (14, 15).









orthotopic tumor models. First, establishment of the blood supply might be much more critical at the newly forming metastatic sites relative to the established primary tumor, creating a differential sensitivity to the targeted treatment. Second, we demonstrate that RGD-Dox-NPs induce apoptosis in the  $\beta$ 3-positive tumor vasculature (Fig. 3C), and this effect on the primary tumor could influence the invasive behavior of the tumor and its ability to metastasize. Third, in the tumor models examined here, to some degree primary tumor growth correlated with metastatic potential. For example, treatment of the pancreatic carcinomas with 7.5 or 15 mg/kg of free Dox reduced both the size of the primary tumor and the metastatic burden in the hepatic hilar lymph node (Fig. 3E). Further studies are necessary to elucidate the mechanism of the antimetastatic effect that might become important for other targeting strategies.

Using NP-mediated Dox delivery to the tumor vasculature, we were able to observe a 15-fold improvement in drug efficacy relative to animals treated with free drug (Fig. 3). Dox is dose-limited by cardiotoxicity (24), and lower doses greatly reduce the side effects of this chemotherapeutic agent. By targeting NPs to the tumor neovasculature, we observed an antitumor effect at 1 mg/kg of NP-encapsulated Dox with no appreciable weight loss, whereas 15 mg/kg of free Dox was required for similar efficacy, leading to an 18% decrease in body weight (Fig. S2). It will be interesting to use this approach with a number of the newer pharmacological agents designed to suppress tumor or vascular cell signal transduction (25). Although some of these agents are beginning to show promise in the clinic, targeted NP delivery would likely reduce the concentration needed for efficacy and minimize problems associated with pharmacokinetics and/or side effects.

## Methods

**Animal Studies.** All animal procedures were conducted in accordance with all appropriate regulatory standards under protocol S05018 and approved by the University of California San Diego Institutional Animal Care and Use Committee.

**Cell Culture.** M21L-GFP melanomas were maintained under standard culture conditions in DMEM supplemented with 10% FBS. R40P cells were isolated and cultured from a spontaneous pancreatic tumor in *Pdx1-Cre,LSL-KRas<sup>G12D</sup>,Ink4a/Arf<sup>lox</sup>* mice after 7 weeks. Both the mice and tumor cell isolation procedure have been described (13). The R40P cells were maintained under standard culture conditions in RPMI medium 1640 supplemented with 10% FBS. SN12C-RFP cells were a gift from Robert Hoffman at AntiCancer, Inc. (San Diego). The SN12C-RFP renal carcinomas were grown in RPMI medium 1640 supplemented with 10% FBS and maintained under standard culture conditions. HUVECs were purchased from Lonza and maintained in EBM-2 with EGM-2 singlequots. HUVECs were propagated on plates coated with 10  $\mu$ g/ml of collagen type I (Millipore), and all experiments were conducted at passage <6.

**Synthesis of Peptide-Lipid Conjugates.** The cyclic peptides, cRGDFK and cRADfK (f denotes D-phenylalanine), were synthesized by using standard Fmoc solid-phase chemistry as described (26). Peptides were purified by reverse-phase HPLC, and exact mass was confirmed by mass spectroscopy. For conjugation to lipid, the peptides were conjugated to a short linker, succinimidyl ester-(PEO)<sub>4</sub>-maleimide (Pierce). DSPE was reacted with iminotriolane (Sigma-Aldrich) to produce a free thiol. The DSPE containing the free thiol group was reacted with the cRGDFK-(PEO)<sub>4</sub>-maleimide or cRADfK-(PEO)<sub>4</sub>-maleimide to produce the peptide-lipid conjugates, and those conjugates were recrystallized in methanol/diethyl ether 1:9 at 4°C overnight. The exact mass of the peptide-lipid conjugates was verified by mass spectroscopy.

**NP Preparation.** The particle formulation of cholesterol/DOPE/DSPE/DSPE-(PEO)<sub>4</sub>-cRGDFK/DSPE-mPEG2000 (6:6:6:1:1 molar ratio) in chloroform was evaporated under argon gas, and the dried lipid film was hydrated in sterile 300 mM ammonium phosphate buffer (pH 7.4) in a total volume of 5 ml at a total lipid concentration of 3.32 mM for a minimum of 1 h. Liposomes were vortexed for 2–3 min to remove any adhering lipid film and sonicated

in a bath sonicator (ULTRASONIK 28X) for 2–3 min at room temperature to produce multilamellar vesicles (MLVs). MLVs were then sonicated with a Ti-probe (Branson 450 sonifier) for 1–2 min to produce small unilamellar vesicles (SUVs) as indicated by the formation of a translucent solution. To reduce the size of the SUVs, stepwise extrusion was performed with the final step being extrusion through a polycarbonate filter with 100-nm pore size (Whatman). The buffer was exchanged with 20 mM HEPES, 150 mM NaCl, pH 7.4 by using gel-filtration chromatography (PD-10; GE Healthcare). Dox (Fluka) encapsulation was performed as described (27) with one slight variation in loading temperature. After addition of Dox to the NPs, the solution was heated at 55°C for 1 h and then left overnight at room temperature before purification by PD-10 column, eluted with water. The amount of encapsulated Dox was quantified by adding 1.5% Triton X-100 to disrupt the NPs and comparing the absorbance at 476 nm on a spectrophotometer to a standard curve of free Dox.

**In Vitro Competition Assay.** HUVECs were seeded and grown overnight in 48-well plates coated with 10  $\mu$ g/ml collagen type I and blocked with 5% BSA. For competition, a 20-fold molar excess of either cRGDFK or cRADfK peptide was preincubated with the cells for 5 min in serum-free medium. NPs containing 1% of a BODIPY 630/650 (Invitrogen)-linked DOPE for fluorescence microscopy were added to the HUVECs for 20 min at 37°C. Cells were fixed and NP binding was visualized by confocal microscopy (Nikon C1si).

**Dorsal Skin-Fold Window Chamber.** Intravital microscopy of NP binding to the tumor neovasculature was monitored in the dorsal skin-fold window chamber as described (21, 22). Two days after surgical implantation of the window chamber, a concentrated (4  $\mu$ l) suspension of 800,000 M21L-GFP melanoma cells was injected into the retractor muscle within the chamber. After 7 days and the appearance of tumor-associated angiogenesis, fluorescent RGD-NPs or RAD-NPs were injected i.v., and the animals were imaged 5 h postinjection by confocal microscopy (Nikon C1si).

**In Vivo Angiogenesis.** The Matrigel assay was performed to assess *in vivo* angiogenesis (10). Briefly, mice were injected s.c. on the flank with 400  $\mu$ l of growth factor-reduced Matrigel (BD Biosciences) containing either sterile saline or 400 ng of human recombinant bFGF (Millipore). After 7 days, mice were injected i.v. with 20  $\mu$ g fluorescein-labeled *G. simplicifolia* lectin that binds selectively to mouse endothelial cells (GSL I-BSL I; Vector Labs). The Matrigel plugs were removed, photographed, viewed whole-mount by confocal microscopy (Nikon C1si), and then fixed and stained for fluorescence microscopy or homogenized, and the fluorescence content was quantified with a fluorimeter by using standard fluorescein filters (Tecan).

**Pancreatic Carcinoma Model.** The orthotopic pancreatic carcinoma model has been described (28, 29). Briefly, 6- to 10-week-old Tie2-GFP mice (30) were injected with 1 million syngeneic murine R40P cells in the tail of the pancreas. NPs containing Dox were injected i.v. on days 5, 7, and 9 postsurgical implantation of the cells. On day 11, the primary tumor and the hepatic hilar lymph node were resected and weighed. To quantify metastasis, the combined weight of both the lymph node and metastatic lesions is reported. Standard immunohistochemistry on frozen sections was performed. Images were acquired by using either a standard light microscope equipped with a CCD camera or confocal microscopy. The  $\beta$ 3 integrin antibody was from BD Biosciences (550541). Blood vessels were labeled for "EC markers" with a mix of rat anti-mouse antibodies recognizing Flk-1 (BD Biosciences; 550549), CD31 (BD Biosciences; 550274), VE-cadherin (BD Biosciences; 555289), and CD105 (Millipore; CBL1358). The Apoptag kit from Millipore (S7165) was used as directed to assess apoptosis on frozen tissue sections. For targeting studies and biodistribution, fluorescent NPs (as described above) were injected on day 11, and the organs were resected at 5-h postinjection. The organs were imaged via whole mount on glass slides by confocal microscopy (Nikon C1si). Fluorescence was observed from both the NP and the blood vessels of the Tie2-GFP mice in which GFP was expressed in the endothelium.

**Renal Cell Carcinoma Model.** The renal cell carcinoma model was used as described (31). One million tumor cells in 20  $\mu$ l of a 1:1 PBS/Matrigel mixture were injected into the lower pole of the kidney just below the renal subcapsule in male nu/nu mice. The needle was removed after a visible blister formed and leakage of the tumor cell suspension was minimal. Animals that formed visible blisters upon injection in the subcapsule with minimal leakage were used for the study. Mice with orthotopic injections of the SN12C-RFP cells were imaged by using the Olympus OV100 Small Animal Imaging System and grouped on day 7 based on weight and imaging results. NPs were injected i.v. every other day beginning on day 8 and continuing until the end of the

