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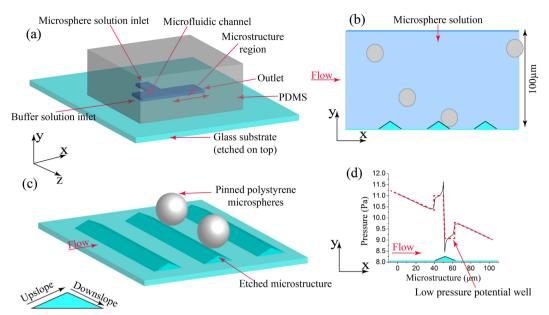
# **OPEN** Trapping/Pinning of colloidal microspheres over glass substrate using surface features

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Suspensions of micro/nano particles made of Polystyrene, Poly(methyl methacrylate), Silicon dioxide etc. have been a standard model system to understand colloidal physics. These systems have proved useful insights into phenomena such as self-assembly. Colloidal model systems are also extensively used to simulate many condensed matter phenomena such as dynamics in a quenched disordered system and glass transition. A precise control of particles using optical or holographic tweezers is essential for such studies. However, studies of collective phenomena such as jamming and flocking behaviour in a disordered space are limited due to the low throughput of the optical trapping techniques. In this article, we present a technique where we trap and pin polystyrene microspheres  $\sim$ 10  $\mu m$  over 'triangular crest' shaped microstructures in a microfluidic environment. Trapping/Pinning occurs due to the combined effect of hydrodynamic interaction and non-specific adhesion forces. This method allows trapping and pinning of microspheres in any arbitrary pattern with a high degree of spatial accuracy which can be useful in studying fundamentals of various collective phenomena as well as in applications such as bead detachment assay based biosensors.

Understanding of collective phenomena such as agglomeration, jamming, glass transition, directed self-assembly is a major research area in mesoscale physics. The underlying physics behind these phenomena occur at a length scale intermediate between atomic and bulk matter. Typically an aqueous solution of micro/nano sized polystyrene or silica particles is used in experimental studies. They interact weakly among themselves through van der Waals, Coulomb and depletion forces. These interactions can be easily tuned by functionalizing the particles<sup>1-3</sup> or changing their chemical environment<sup>4,5</sup>. Therefore, colloidal solutions can be used to study many condensed matter phenomena. In particular, colloidal microspheres have been an excellent model system to gain an understanding of long-standing open issues associated with phase transitions in glassy systems, for instance, the role of quenched disorder in glass transition<sup>6–8</sup>. In general, the role of disorder in a variety of collective phenomena has attracted recent interest. For instance, researchers are studying collective behaviour of active particles in disordered media motivated by the desire to understand motility of living organisms such as bacteria in real environments<sup>9-11</sup>. A relatively simple way to create disordered energy landscapes to study such phenomena is by trapping or pinning particles at desired spatial locations. Conventionally, an optical tweezer is used to trap and manoeuvre such particles<sup>12,13</sup>. Recently, researchers have shown trapping of microspheres in microfluidic environment by various strategies such as the creation of eddies using oscillating flow around obstruction<sup>14</sup>, fluid flow from multiple directions to create low pressure region 15, use of rotating magnetic rod to create vortex 16. Though these systems are very useful, they have certain limitations. The applicability of an optical tweezer is limited by the laser intensity which a sample can withstand. Trapping methods based on hydrodynamics require very specific settings in each case, and hence lacks versatility. In general, the trapping methods developed so far have a low throughput, which fundamentally restricts the study of collective phenomena. To address the issue of throughput, modification such as holographic optical tweezers have been used to create pinning patterns<sup>17,18</sup> but, the number of optical traps which can be generated is limited, typically of the order of  $\sim 100^{19}$ . The techniques developed as yet are largely non-contact, presumably to provide a pristine system for experiments. However, a non-contact mode of trapping may not be a critical requirement for many experiments in colloidal physics. The contact mode of trapping can be done by flowing functionalized particles over a chemically patterned substrate where particles get pinned due to the formation of a chemical bond<sup>20-22</sup>. A contact mode of trapping such as the one mentioned

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\*Figure not to scale

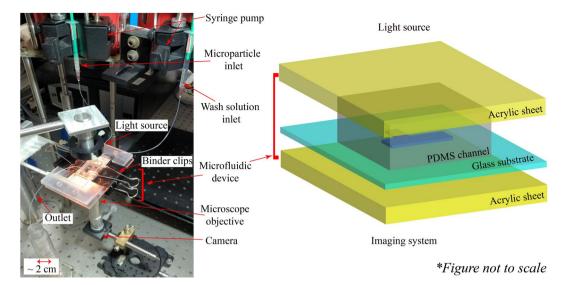
**Figure 1.** Schematic of a PDMS microfluidic channel clamped over an etched glass substrate. (a) T-shaped microfluidic channel with two inlets, one for microsphere solution and other for the plain buffer solution. (b) Side view of microfluidic channel showing pinned polystyrene microspheres. Channel has a width of  $500 \, \mu m$  (z–axis) and a depth of  $100 \, \mu m$  (y–axis), length of the entire channel is  $1 \, cm$  (x–axis). (c) Top view of the pinned polystyrene microspheres over etched microstructure. (d) The simulated pressure profile over the microstructured glass substrate of height  $4 \, \mu m$  and width  $20 \, \mu m$  at the bottom of the channel. It was calculated by setting up the Navier-Stokes equation for an incompressible fluid flow at a flow rate of  $50 \, \mu l/min$ .

above requires multiple steps of chemical patterning which makes the process tedious and less versatile. However, such methods enable the creation of well defined pinning patterns of particles which are necessary to understand the effect of disorder in collective behavior. The complexity of chemical approaches to create pinning patterns prompted us to consider a purely physical approach towards contact-mode of trapping (In this article, we use the terms trapping and pinning synonymously). Specifically, we explored the ability of microstructured surface<sup>23–25</sup> features to trap/pin microspheres using static potential wells generated by near-field flow effects from microstructures inside a microfluidic channel. We demonstrate, in this article, a simple process to create an arbitrary 2D pattern of pinned particles using microstructures whose height could be as low as 1/10<sup>th</sup> of that of the particles.

The adhesion force between 5–10  $\mu m$  polystyrene microspheres and the glass substrate is of the order of 1–100  $nN^{26,27}$ . In comparison, force due to gravity on the microspheres in aqueous medium is less than 1 pN. At such range of adhesion strengths, microspheres can be reliably pinned if they come in contact with the substrate surface. The flow of an aqueous solution over a microstructured substrate having a shape of triangular crest in a microfluidic channel leads to a formation of static low pressure region around it (Fig. 1(d)). Microsphere laden flow over such a substrate in a microfluidic channel leads to particles getting pinned in the low pressure region around the triangular crests. We found such structures to be very conducive for reliable trapping/pinning of microspheres of diameter as low as 5  $\mu$ m. We have shown, robust trapping/pinning over a crest of height as low as ~1  $\mu$ m, in comparison, the microsphere diameter was 5  $\mu$ m & 10  $\mu$ m. We further explored the critical role of microstructure geometry and flow rate in reliable trapping/pinning of particles which is supported by fluid dynamics simulation using the finite element method (FEM) implemented in COMSOL, a commercial numerical package. The technique described here offers a simple method to trap and pin polystyrene particles in 2D patterns with minimal complexity and can be easily scaled up.

# **Materials and Methods**

**Channel design and trapping principle.** A schematic of the microfluidic channel used for the experiments is shown in Fig. 1(a). A PDMS channel is clamped onto an etched glass slide which was fabricated by an isotropic hydrofluoric acid (HF) etch of a photoresist patterned substrate. The channel has two inlets, one for the microsphere solution and the other for the Phosphate Buffered Saline (PBS buffer) solution to generate shear force by means of the fluid flow. Polystyrene microspheres sized  $5 \, \mu m \, \& \, 10 \, \mu m$  in  $0.01 \, M$  PBS buffer solution were flown through the microsphere solution inlet. As they flow past near the crests they get pinned in the low pressure region (Fig. 1(d)) by adhering to the substrate as depicted in Fig. 1(b,c). The probability of a particle getting trapped in the upslope or downslope regions depends on the flow rate. At high flow rates, particles are predominantly pinned in the downslope region while at a very low flow rate pinning can be also seen in upslope region.



**Figure 2.** Schematic of the experimental setup: A microfluidic channel made up of PDMS and glass substrate is sandwiched between the top and bottom layer of acrylic sheet and the whole assembly is clamped tightly using binder clips. Device is illuminated from the top and imaged from the bottom using 20x & 40x microscope objective along with a CMOS camera assembly.

**Experimental setup.** A T-shaped Polydimethylsiloxane (PDMS) microfluidic device with a channel depth of  $100 \, \mu m$ , width  $500 \, \mu m$  and length  $1 \, cm$  was cured over a SU8 mould fabricated using photolithography process. The microfluidic device was assembled by clamping PDMS channel on the microstructured glass substrate using binder clips (Fig. 2), and observed using an inverted imaging setup where the device was illuminated from the top and imaged from the bottom.

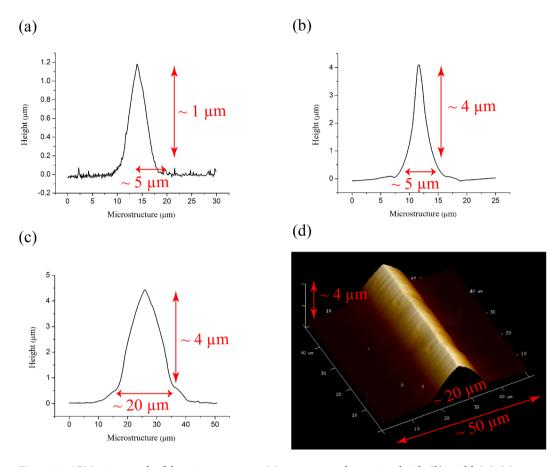
**Fabrication of the microfluidic channel.** A  $100~\mu m$  thick layer of negative resist SU-8 2100 was spin coated on a silicon wafer and then patterned using photolithography technique. Subsequently, it was developed to achieve a  $500~\mu m$  wide,  $100~\mu m$  thick and 1~cm long T-shape mould. The channel was fabricated by pouring PDMS and curing agent in the ratio of 10:1 over the mould and was cured at a temperature of 100 °C for an hour. After curing, the microfluidic channel was peeled off and the inlet/outlet holes were punched using a biopsy punch.

**Fabrication of microstructure.** The role of microstructure in trapping and pinning of polystyrene microsphere is determined by performing the experiments on microstructures of various heights and widths (Fig. 3). Commonly available microscopic glass slides of dimension  $75 \,\mathrm{mm} \times 25 \,\mathrm{mm}$  and thickness of  $1 \,mm$  were used as a substrate. Resist patterned glass slides were isotropically etched using a mixture of 50% HF, 36% HCl and Deionized(DI) water in the ratio 1:1:3. HF etches out various silicon oxides present in the glass slide while HCl removes metal contents sodium and calcium respectively. This mixture gives an etch rate of about  $100 \,\mathrm{nm/s}$ . As wet etching is an isotropic process, it etches out the glass substrate in transverse as well as lateral direction. Lateral etching was controlled to some extent by optimising the post-development baking time of photoresist. We used positive photoresist S1813 for microstructures with depth  $1-2 \,\mu m$  and AZ4562 for even larger depths which resulted in an optimal etching and resist stripping process. Figure 3 shows the Atomic Force Microscopy (AFM) micrograph of three microstructures with different dimensions used for the experiments.

The etch time and chemicals used for fabricating microstructures are mentioned in Supplementary Table 1. We fabricated an array of the microstructures of different dimensions as shown in Fig. 3(a,b,c) with a periodicity of  $50 \, \mu m$ ,  $50 \, \mu m$  &  $100 \, \mu m$  respectively.

The microstructure of smaller height, as shown in Fig. 3(a), was fabricated by using photoresist S1813, it was coated @ 2000 rpm over glass substrate which provides a uniform resist thickness of about  $2.2 \,\mu m$ . Subsequently, the resist was photo-lithographically patterned to get an array of width  $5 \,\mu m$  and periodicity  $50 \,\mu m$  over the substrate. A post-development bake of  $3 \,min$  @  $110 \,^{\circ}$ C was done before dipping it in the HF etchant for  $10 \,sec$  to etch out the bare glass portion. Similarly for the triangular crest structure of larger dimensions as shown in Fig. 3(b and c), the substrate was coated with AZ4562 @  $4000 \,rpm$  providing a resist thickness of about  $6.2 \,\mu m$  which was then patterned to get a resist array of width  $5 \,\mu m \,\&\, 20 \,\mu m$  respectively. A post-development bake of  $5 \,min$  @  $110 \,^{\circ}$ C was done before dipping it in the etchant solution for  $40 \,sec$  to get an array of microstructures. The residual resist was removed by the sonication of substrate in acetone. The microstructured glass substrate was further cleaned in piranha solution  $(3H_2SO_4 + 1H_2O_2)$  before the experiment. A roughness measurement over 5 glass substrate using Bruker AFM tapping mode revealed little change post etching. The average roughness pre and post etching where about  $7.8 \,nm$  and  $8.3 \,nm$  respectively.

**Chemicals and microsphere solution.**  $10 \,\mu m \,\&\, 5 \,\mu m$  Polystyrene microspheres were purchased from Sigma-Aldrich. They were rinsed using DI water and diluted to  $10 \,mg$  per ml using Phosphate Buffered Saline (PBS)  $0.01 \,M$ . PBS buffer was prepared by mixing PBS tablets from Sigma-Aldrich in DI water and has a pH of 7.4



**Figure 3.** AFM micrograph of the microstructures. Microstructure dimension: height(h), width(w). (a)  $h=1.1~\mu m, w=5.1~\mu m$ . (b)  $h=4.1~\mu m, w=5.4~\mu m$ . (c)  $h=4.3~\mu m, w=19.2~\mu m$ . (d) Three-dimensional AFM micrograph of the microstructure of  $h=4.3~\mu m, w=19.2~\mu m$ .

at 25 °C. The number of  $10 \,\mu m \,\&\, 5 \,\mu m$  particles in solution is of the order of  $10^6 \,\&\, 10^7 \,\mathrm{per} \,ml$  respectively.  $0.1 \,ml$  of microsphere solution was used in a single experiment.

**Numerical simulation of pressure profile over crests.** The pressure profile in the channel was calculated by solving the Navier-Stokes equation (Equation 1) corresponding to incompressible flow for which  $d\rho/dt = 0$ , which is equivalent to Equation 2.

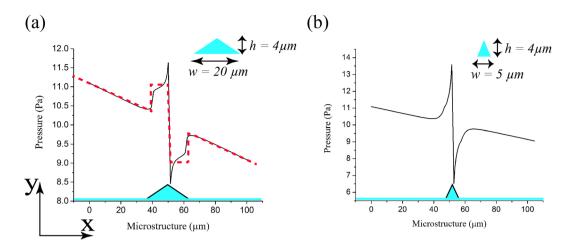
Navier – Stokes Equation: 
$$\rho \frac{\partial u(t)}{\partial t} + \rho(u \cdot \nabla u) = -\nabla p + \mu \nabla^2 u$$
 (1)

Continuity Equation: 
$$\nabla \cdot u = 0$$
 (2)

where  $\rho$  &  $\mu$  is the density and dynamic viscosity of the solution. A two-dimensional schematic of the channel is shown in Fig. 1(c), where, no-slip boundary condition (u=0) is applied at the top and bottom surface along with an inflow and outflow condition depending upon the flow rate ( $u=u_{avg}$ ) at the inlet and outlet of the channel respectively Figure 4 shows the simulated pressure profile arising from fluid flow across a microstructure. A low pressure potential well can be seen in the upslope and downslope region of the triangular crest. At a very low flow rate polystyrene microspheres get pinned in the upslope region simply because the microstructure acts as a barrier to their flow. However, at a higher flow rate, polystyrene microspheres accelerate as they flow through the upslope region due to decrease in cross-sectional channel volume. As a result they acquire a velocity in +y direction thus moving away from the substrate resulting in no pinning. On the contrary, in the downslope region microspheres decelerate due to increase in the channel volume and acquire a velocity in -y direction thus moving towards the substrate which results in an increased probability of pinning. Surface plots of the velocity vector are shown in Supplementary Fig. S1.

Pressure profile over microstructures of different shapes is shown in Supplementary Fig. S2. We focussed on the 'triangular shaped crests' as they can be easily fabricated using isotropic etch of glass substrate.

**Estimation of adhesion force between microsphere and glass substrate.** Non-specific forces such as the van der Waals and electrostatic double layer interaction force, collectively known as the DLVO force, exist between any two surfaces. At macro-scale, their effect is minuscule and not readily observable. However, they can



**Figure 4.** Pressure profile plots over the surface of microstructure with different geometries showing low pressure region around crest. Volumetric flow rate was  $50 \,\mu l/min$  and the channel domain was considered to be  $1 \,mm$  long instead of  $1 \,cm$  to save the computation cost. Microstructure dimension: height "h", slopewidth (upslope + downsloperegion - "<math>w") (a)  $h = 4 \,\mu m$ ,  $w = 20 \,\mu m$ . (b)  $h = 4 \,\mu m$ ,  $w = 5 \,\mu m$ .

be prominent at micro scale. Microsphere detachment experiments using fluidic shear force was done on plain glass substrates to estimate the adhesion strength<sup>27–29</sup>. Polystyrene microspheres of size  $5 \mu m \& 10 \mu m$  were flown along with buffer solution through the microsphere inlet. After sustaining a stable flow, the flow was stopped so that the microspheres can settle on the bottom of the substrate. Velocity in the downward direction due to the gravitational force of a 10  $\mu m$  sized microsphere is around 2.75  $\mu m/s$  and therefore it would take about a minute for all the microspheres to settle. The 5  $\mu m$  particles have a downward velocity of about 0.69  $\mu m/s$  and take a longer time to settle. After a 5 minute of incubation period, PBS buffer solution was flown through the buffer inlet and the flow rate was increased until the viscous drag was enough to detach the particles. We saw no detachment up to a flow rate of 500 μl/min and 300 μl/min for microspheres sized 5 μm & 10 μm respectively in the experiment done on five different glass substrates. The microsphere is assumed to be static and the no slip boundary condition is applied on the channel surface as well as on the microsphere to estimate the shear force using simulation, as described in previous section. The viscous drag on microspheres sized 5  $\mu m \& 10 \mu m$  adhered to the bottom surface of the channel comes out to be 1.88 nN & 4.6 nN respectively which matches well with the analytical estimation explained in supplementary text. The larger drag force on the microsphere sized  $10 \, \mu m$  even at a lower flow rate is due to the parabolic flow profile in a rectangular channel. The flow rate in the entire experimental analysis is less than  $100 \,\mu l/min$ , well within the upper limit of microsphere detachment flow rate of  $300 \,\mu l/min$ .

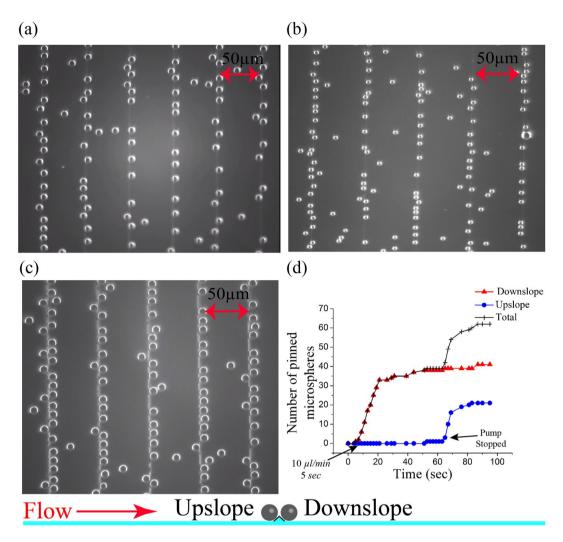
**Data availability.** Data and videos are available on the request from the corresponding author.

#### **Results and Discussion**

The density of polystyrene is  $1.05\,gm/cm^3$  while that of water is  $1.0\,gm/cm^3$ . Hence, in an aqueous medium, they move downward due to the gravitational force. If these particles are pumped in a microfluidic channel over a plain glass substrate and left idle for some time they will randomly settle within the channel and can be reliably pinned. However, if they are pumped continuously they won't pin at all. Even at a low flow rate of  $5\,\mu l/min$ , the microspheres simply glide over the substrate and are flushed out. We have used an array of microstructures to demonstrate high throughput trapping/pinning of polystyrene microspheres. Figure 5(a & b) shows pinned microspheres of diameter  $10\,\mu m \& 5\,\mu m$  respectively on the microstructures of smaller dimension  $(h=1.1\,\mu m,w=5.1\,\mu m)$ . The microspheres typically pin at flow rates less than  $50\,\mu l/min$ , pinned microspheres as shown in Fig. 5(a,b and c) is achieved by stopping the flow for  $30-40\,sec$  at a high flow rate of  $50\,\mu l/min$  which results in a high throughput. A real-time video of trapping/pinning of particles is shown in the movie "supple\_pinning1.mov" provided as a supplementary data.

Figure 5(d) shows the number of pinned microsphere as the time progresses. Initially, the flow rate is  $50 \,\mu l/min$  which is reduced to  $10 \,\mu l/min$  at  $t=5 \,sec$  resulting in the pinning ar the downslope region which saturates after some time due to a decrease in the number of empty sites. Later, the pump is stopped at  $t=60 \,sec$ , as the speed further decreases microspheres starts filling the upslope region. Microsphere sized  $10 \,\mu m$  has a velocity of  $\sim 2.75 \,\mu m/s$  in the downward direction, at this velocity it takes roughly  $0.35 \,sec$  for the particles to cover a distance of  $1 \,\mu m$  which is the height of microstructure shown in Fig. 5(a and b). The periodicity of the microstructure is  $50 \,\mu m$ , hence, velocity of microspheres sized  $10 \,\mu m$  along the channel should be  $145 \,\mu m/s$  (volumetric flow rate  $= 18 \,\mu l/min$ ), such that it encounters the successive crest before touching the substrate surface. This condition gives a lower limit of the flow rate for a precise pinning in the downslope region.

**Pinning efficiency of the microstructured substrate.** Figure 6(a and b) shows the histogram of pinned microsphere of size  $10 \, \mu m$  cumulated over six microstructures which we were able to image at once. The length of each microstructure is  $360 \, \mu m$ , hence, at the most  $36 \, \text{microspheres}$  can be pinned along each microstructure. If we assume that on an average pinned microspheres are equally spaced then roughly half of the sites can't be



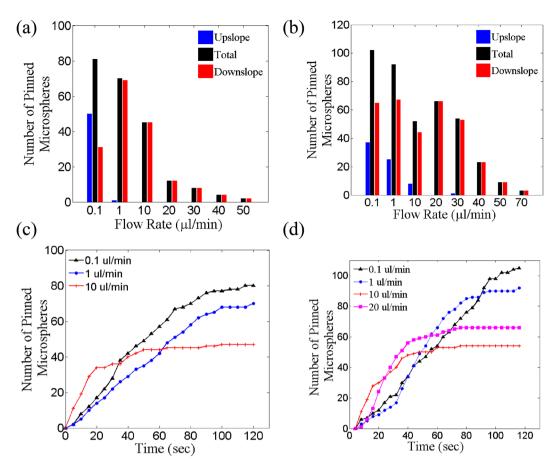
**Figure 5.** Images of pinned microspheres on an array of microstructures. (a) Microspheres of diameter  $10 \, \mu m$  pinned on the microstructure of  $h = 1.1 \, \mu m$ ,  $w = 5.1 \, \mu m$ . (Fig. 3a). (b) Microspheres of diameter  $5 \, \mu m$  pinned on the microstructure of  $h = 1.1 \, \mu m$ ,  $w = 5.1 \, \mu m$  (Fig. 3a). (c) Microspheres of diameter  $10 \, \mu m$  pinned on the microstructure of  $h = 4.1 \, \mu m$ ,  $w = 5.4 \, \mu m$ . (d) A plot of number of pinned microsphere vs time in the upslope and downslope region cumulated over five microstructure of  $h = 1.1 \, \mu m$ ,  $w = 5.1 \, \mu m$ .

occupied and hence a total of  $18 \times 6 = 96$  sites are available. From the histograms in Fig. 6(a and b) we can see that up to 100% of the sites can be filled within two minutes under appropriate conditions. Furthermore, as the height is increased from  $1.1 \, \mu m$  in Fig. 6(a) to  $4.1 \, \mu m$  in Fig. 6(b) microspheres can be pinned even at a higher flow rate.

Figure 6(c and d) shows the number of pinned microspheres with time at different flow rates. The number of pinned microspheres rises linearly and persists with time for flow rates below  $1 \,\mu m$  whereas it saturates quickly after increasing linearly at higher flow rates  $\geq 10 \,\mu l/min$ . The microspheres pin at low flow rates  $\leq 1 \,\mu l/min$  in upslope region because the crests act as a gravitational potential barrier. A real time video "supple\_pinning2.mov" is provided which shows pinning of microsphere in the upslope region (t=0-15 sec) at a low flow rate of  $0.1 \,\mu l/min$  on the microstructure of  $h=1.1 \,\mu m$ ,  $w=5.1 \,\mu m$ . Velocity of the microspheres which were pinning in the upslope region was in the range of  $6-18 \,\mu m/s$  as estimated from the video analysis.

**Pinning of microspheres at a high flow rate over larger microstructure.** Robust pinning at a high flow rate of  $50 \,\mu l/min$  is achieved on the larger microstructures of  $h = 4.3 \,\mu m, w = 19.2 \,\mu m$  as shown in Fig. 7(a and b). The drag force on the pinned microspheres as depicted in Fig. 7(d) is  $\sim 0.83 \, nN$  which is much lower than the upper limit of shear detachment force  $\sim 4.6 \, nN$  at a flow rate of  $300 \,\mu l/min$ .

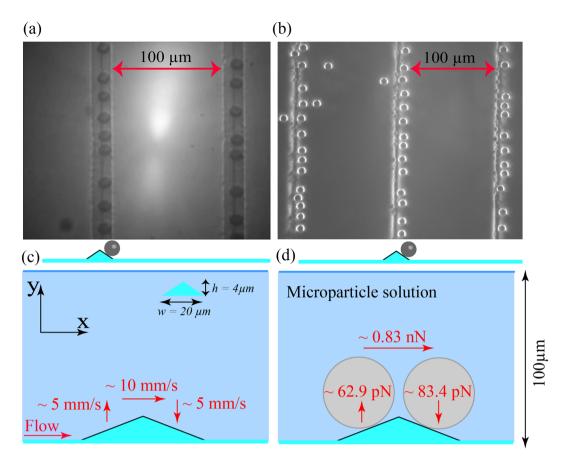
We can see from the histogram in the Fig. 6(b) that very few microspheres are pinned at a flow rate of  $50 \,\mu l/min$  on the microstructure of  $h=4.1 \,\mu m, w=5.4 \,\mu m$ . However, considerable pinning is seen as the width of the microstructure is increased from  $5.4 \,\mu m$  to  $19.2 \,\mu m$ , as shown in Fig. 7(a and b). Hence, trapping/pinning can be achieved at a high flow rate either by increasing the height or the width of the microstructure. A microsphere on the top of the microstructure flows with an average velocity of  $10 \, mm/s$  as depicted in Fig. 7(c), whereas the microstructure width is nearly  $20 \,\mu m$ . The average transit time of the particle across the microstructure is only  $2 \, ms$ . The kinetic arrest of microspheres having such high momentum has not been previously reported. Previous



**Figure 6.** Histogram of the number of pinned microspheres at different flow rates in 2 minute for microstructure (a)  $h = 1.1 \, \mu m$ ,  $w = 5.1 \, \mu m$ ; (b)  $h = 4.1 \, \mu m$ ,  $w = 5.4 \, \mu m$ . Graph of number of pinned microspheres vs time at different flow rate for microstructure (c)  $h = 1.1 \, \mu m$ ,  $w = 5.1 \, \mu m$ ; (d)  $h = 4.1 \, \mu m$ ,  $w = 5.4 \, \mu m$ .

reports on the kinetic arrest of microspheres were shown using holographic tweezers where the velocity of the microsphere is of the order of  $\sim 100 \, \mu m/s$  with a trapping power of  $150 \, \mu W^{19}$ .

**Explanation of trapping/pinning at a high flow rate.** The flow in a microfluidic channel follows a laminar profile even at a high flow rate of 50  $\mu$ l/min due to low Reynolds number of the channel,  $R_c = \rho u l / \mu \approx 2$  $(\rho = 1 \text{ g/cm}^3 \text{ is the density}, u = 0.016 \text{ m/s} \text{ is the average velocity}, u = 0.001 \text{ kg} \cdot \text{m}^{-1} \cdot \text{s}^{-1} \text{ is the dynamic viscosity}$ and  $l = 100 \, \mu m$  is the height of the channel). Microsphere inertia while moving past the microstructure can also be ignored since the lag time of microsphere  $\tau_b = 2r^2\rho_b/9\mu \approx 2\,\mu s$  ( $r = 5\,\mu m$  is the radius,  $\rho_b = 1.05\,gm/cm^3$  is the density of particle) is much less than the characteristic disturbance time  $a/U \sim 1 ms$  ( $a = 10 \mu m$  is the length of downslope region and  $U=10 \, mm/s$  is the average velocity of microsphere near the crests). The ratio  $\tau_p U/a \approx$ 0.002 is known as the Stokes number, a low value of which indicates that the microsphere will respond almost instantaneously to the flow rate<sup>30</sup>. Inertial migration due to the parabolic flow profile can also be neglected since the microsphere Reynolds number  $R_p = R_c r^2 / l^2 \ll 1^{31,32}$ . We further carried out experiments using surfactant solution 0.1% PBST, which did not result in any pinning. Therefore, trapping due to the formation of local vortices or any other fluid dynamical effects can be ruled out. Thus, we can convincingly argue that the pining of the microspheres is due to the non-specific binding occurring after they come sufficiently close to the substrate due to the hydrodynamic interaction. As the microsphere flows past the crest a sudden increase in channel volume results in low pressure in the downslope region, in other words the flow field decelerates and diverges bringing the microspheres closer to the substrate. The microspheres which are close enough will start experiencing hydrodynamic interaction with the glass substrate and gets pinned due to van der Waals interaction force. The prominent interaction forces between a spherical object and glass substrate are van der Waals and electrostatic double layer interaction force, collectively known as DLVO force. Van der Waals force between a spherical object and a flat surface is  $F_V = -AR/6D^2$ , where, A is Hamaker constant and R & D are the radius of the microsphere and its distance from the substrate respectively. The electrostatic force between a spherical object and a flat surface of similar potential is  $F_E = 2\pi R W_{flat}$ , where, R is the radius of the microsphere and  $W_{flat} = 0.0211 \, (C)^{1/2} \, \tanh^2 \left[ 2\varphi(mV)/103 \right] e^{-D/l_d} Jm^{-2}$  is the interaction free energy, D is the distance of microsphere from the substrate and  $l_d$  is the screening length also known as the Debye length. The Hamaker constant is of the order of  $A = 1 \times 10^{-20} J^{33}$  and the Debye length  $l_d$  is of the order of 1.5 nm, the calculation of the Debye length and other parameters is explained in the supplementary text. The polystyrene microsphere has a Zeta potential of around -40 mV in 0.01 M PBS buffer at a pH of 7.5<sup>34</sup> whereas the Zeta potential of fused silica



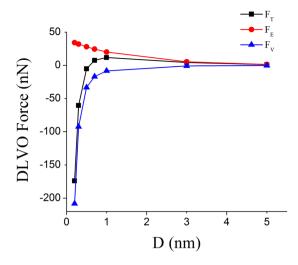
**Figure 7.** Pinning at high flow rates over the microstructure of  $h=4.3~\mu m, w=19.2~\mu m$ . (a) Bright field expanded image of pinned microspheres of size  $10~\mu m$  on the downslope region of microstructure  $h=4.3~\mu m, w=19.2~\mu m$ . (b) Dark field image of  $10~\mu m$  microspheres preferentially pinned on the downslope region of microstructure  $h=4.3~\mu m, w=19.2~\mu m$ . (c) Average velocity along the channel just above the microstructure is 10~mm/s whereas in upslope and downslope region, it is 5~mm/s in (+~y) and (-y) direction respectively. (d) Microsphere of size  $10~\mu m$  pinned in upslope region experiences a lift force of 62.9~pN thus opposing the adhesion whereas in the downslope region, a force of 83.4~pN is experienced in the (-y) direction, hence assisting the adhesion. Drag force along the flow at both upslope and downslope region is nearly 0.83~nN.

 $(amorphousSio_2)$  is around  $-60\,mV$  in  $0.01\,M$  KCl solution at a pH of  $7.5^{35}$ . Hence, we have assumed an average potential of  $\phi = -50.0\,mV$ . Figure 8 shows the distance dependence of van der Waals interaction force  $F_{\nu}$ , electrostatic double layer force  $F_E$  and the total force  $F_T$  for a microsphere of radius  $R = 5\,\mu m$ .

As the distance between microsphere and the substrate decreases the attractive van der Waals force increases much faster than the repulsive electrostatic force which results in the pinning. The van der Waals force dominates in sub-nanometre length scale which is the reason of the robust pinning of the microsphere. The distance between two surface in contact is  $\sim 0.2 \, nm^{33}$  the respective  $F_v = -206.25 \, nN$  which is much larger than the drag force generated by the flow in the pinning regime that is below 1 nN in all cases. The calculated van der Waals force  $F_v = -206.25 \, nN$  is of the similar order as experimentally measured using AFM<sup>26</sup>. However, in the experiments which we performed, all the pinned microsphere detach at a flow rate of 1-2 ml/min which corresponds to a drag force of 15-30 nN. This decrease is because, in a bead detachment experiment the microspheres are peeled off<sup>27</sup> rather than the transverse detachment as in the case of AFM based techniques<sup>26</sup>. Furthermore, we have also noticed the switching of pinned polystyrene microspheres from upslope region to downslope region. Initially, all the microspheres shown in the video "supple\_pinning3.mov" were pinned in the upslope region of the microstructure  $(h = 4.1 \,\mu m, w = 5.4 \,\mu m)$  at a low flow rate of  $0.1 \,\mu l/min$ . As the flow rate is increased to  $30 \,\mu l/min$ , they switch to downslope region. Hence, the hydrodynamic interaction has an important role in facilitating robust pinning in the downslope region. In summary, the pinning on the upslope region occurs at a low flow rate because upslope acts as a barrier to particle flow whereas, pinning on the downslope region at a high flow rate is facilitated by the hydrodynamic interaction between the microsphere and substrate.

# Conclusion

We have presented a technique where near-field effects due to fluid flow past a microstructure in a channel assist the trapping and pinning of microspheres in a predictable manner. This technique enables a high-throughput production of pinned particles in any desired 2D pattern such as the chequered pattern shown in supplementary Fig. S3. However, unlike the optical tweezer based method, the trapping pattern cannot be made dynamic



**Figure 8.** The van der Waals force  $F_V$ , the electrostatic force  $F_E$  and the total DLVO force  $F_T$  as a function of distance from the substrate for a microsphere of radius 5  $\mu m$ .

in this technique. This method works for the polystyrene microspheres larger than  $5\,\mu m$ , smaller microspheres can't be reliably pinned due to the thermal fluctuations. Nevertheless, the simple approach presented here enables the creation of a large number of pinned microspheres useful in the study of disorder in the dynamics of multi-particle interacting systems. The result from the experiment and simulation suggests that the trapping/pinning of microsphere is due to the combined effect of fluid dynamics and DLVO adhesion forces. A more quantitative analysis of many body colloidal hydrodynamics is indeed required to understand the hydrodynamic interactions. Apart from fundamental studies, pinned microspheres can also be used for molecular sensing as shown in the recent work describing a biosensor with attomolar sensitivity using a configuration of chemically patterned microspheres for detection<sup>36</sup>.

# References

- 1. Kim, A. J., Biancaniello, P. L. & Crocker, J. C. Engineering DNA-Mediated Colloidal Crystallization. Langmuir 22, 1991–2001 (2006).
- 2. Zhong, Z., Patskovskyy, S., Bouvrette, P., Luong, J. H. T. & Gedanken, A. The Surface Chemistry of Au Colloids and Their Interactions with Functional Amino Acids. *The journal of Phy. Chem. B* 108, 4046–4052 (2004).
- 3. Biancaniello, P. L., Kim, A. J. & Crocker, J. C. Colloidal Interactions and Self-Assembly Using DNA Hybridization. *Phys. Rev. Lett.* **94**, 58302 (2005).
- 4. Liang, Y., Hilal, N., Langston, P. & Starov, V. Interaction forces between colloidal particles in liquid: Theory and experiment. *Adv. Colloid Interface Sci.* **134–135**, 151–166 (2007).
- Tohver, V., Smay, J. E., Braum, E., Braum, P. V. & Lewis, J. A. Nanoparticle halos: A new colloid stabilization mechanism. Proc. Natl. Acad. Sci. USA 98, 8950–8954 (2001).
- Hima Nagamanasa, K., Gokhale, S., Sood, A. K. & Ganapathy, R. Direct measurements of growing amorphous order and non-monotonic dynamic correlations in a colloidal glass-former. Nat. Phys. 11, 403–408 (2015).
- 7. Lu, P. J. & Weitz, D. A. Colloidal Particles: Crystals, Glasses, and Gels. Annu. Rev. Condens. Matter Phys. 4, 217-233 (2013).
- 8. Yunker, P., Zhang, Z. & Yodh, A. G. Observation of the Disorder-Induced Crystal-to-Glass Transition. *Phys. Rev. Lett.* **104**, 15701 (2010).
- Reichhardt, C. & Olson Reichhardt, C. J. Active matter transport and jamming on disordered landscapes. Phys. Rev. E. 90, 012701 (2014).
- 10. Morin, A., Cardozo, D. L., Chikkadi, V. & Bartolo, D. Self-propulsion through disorder. arxiv: 1702.07655 (2017).
- 11. Brown, A. T. et al. Swimming in a crystal. Soft Matter 12, 131-140 (2016).
- 12. Ashkin, A., Dziedzic, J. M., Bjorkholm, J. E. & Chu, S. Observation of a single-beam gradient force optical trap for dielectric particles. Opt. Lett. 11, 288 (1986).
- 13. Dienerowitz, M., Mazilu, M. & Dholakia, K. Optical manipulation of nanoparticles: a review. J. Nanophotonics 2, 21875 (2008).
- 14. Lieu, V. H., House, T. A. & Schwartz, D. T. Hydrodynamic Tweezers: Impact of Design Geometry on Flow and Microparticle Trapping. *Anal. Chem.* 84, 1963–1968 (2012).
- Tanyeri, M. & Schroeder, C. M. Manipulation and Confinement of Single Particles Using Fluid Flow. Nano Lett. 13, 2357–2364 (2013).
- 16. Petit, T., Zhang, L., Peyer, K. E., Kratochvil, B. E. & Nelson, B. J. Selective Trapping and Manipulation of Microscale Objects Using Mobile Microvortices. *Nano Lett.* 12, 156–160 (2012).
- 17. Curtis, J. E., Koss, B. A. & Grier, D. G. Dynamic holographic optical tweezers. *Opt. Commun.* **207**, 169–175 (2002).
- 18. Grier, D. G. A revolution in optical manipulation. *Nature* **424**, 810–816 (2003).
- 19. Korda, P. T., Taylor, M. B. & Grier, D. G. Kinetically Locked-In Colloidal Transport in an Array of Optical Tweezers. *Phys. Rev. Lett.* 89, 128301 (2002).
- 20. Sivagnanam, V., Song, B., Vandevyver, C. & Gijs, M. A. M. On-Chip Immunoassay Using Electrostatic Assembly of Streptavidin-Coated Bead Micropatterns. *Anal. Chem.* **81**, 6509–6515 (2009).
- 21. Kim, J. et al. Integrated microfluidic bioprocessor for solid phase capture immunoassays. Lab Chip 11, 3106 (2011).
- 22. Mulvaney, S. P. et al. Rapid, femtomolar bioassays in complex matrices combining microfluidics and magnetoelectronics. *Biosens. Bioelectron.* 23, 191–200 (2007).
- 23. Vogel, N., Retsch, M., Fustin, C. A., del Campo, A. & Jonas, U. Advances in Colloidal Assembly: The Design of Structure and Hierarchy in Two and Three Dimensions. *Chem. Rev.* 115, 6265–6311 (2015).
- 24. Cui, Y. et al. Integration of Colloidal Nanocrystals into Lithographically Patterned Devices. Nano Lett. 4, 1093-1098 (2004).

- 25. Varghese, B. et al. Size Selective Assembly of Colloidal Particles on a Template by Directed Self-Assembly Technique. Langmuir 22, 8248–8252 (2006).
- 26. Xu, Q. et al. Dynamic Adhesion Forces between Microparticles and Substrates in Water. Langmuir 30, 11103-11109 (2014).
- 27. Cho, K. L. et al. Shear-Induced Detachment of Polystyrene Beads from SAM-Coated Surfaces. Langmuir 31, 11105-11112 (2015).
- 28. Cozens-Roberts, C., Quinn, J. A. & Lauffenberger, D. A. Receptor-mediated adhesion phenomena. Model studies with the Radical-Flow Detachment Assay. *Biophys. J.* **58**, 107–125 (1990).
- 29. Javanmard, M., Babrzadeh, F. & Davis, R. W. Microfluidic force spectroscopy for characterization of biomolecular interactions with piconewton resolution. *Appl. Phys. Lett.* **97**, 14–17 (2010).
- 30. Kirby, B. Micro- and nanoscale fluid mechanics: transport in microfluidic devices (Cambridge University Press, 2010).
- 31. Di Carlo, D., Irimia, D., Tompkins, R. G. & Toner, M. Continuous inertial focusing, ordering, and separation of particles in microchannels. *Proc. Natl. Acad. Sci. USA* **104**, 18892–7 (2007).
- 32. Wu, L., Guan, G., Hou, H. W., Bhagat, A. A. S. & Han, J. Separation of Leukocytes from Blood Using Spiral Channel with Trapezoid Cross-Section. *Anal. Chem.* 84, 9324–9331 (2012).
- 33. Israelchvili, N. J. Intermoleculat and Surface Forces (Elsevier, 2009).
- Lundqvist, M. et al. Nanoparticle size and surface properties determine the protein corona with possible implications for biological impacts. Proc. Natl. Acad. Sci. USA 105, 14265–14270 (2008).
- 35. Scales, J. P. et al. Electrokinetics of the silica-solution interface: a flat plate streaming potential study. Langmuir 8, 965–974 (1992).
- 36. Tekin, H. C., Cornaglia, M. & Gijs, M. A. M. Attomolar protein detection using a magnetic bead surface coverage assay. *Lab Chip* 13, 1053–9 (2013).

# **Author Contributions**

P.P. and M.V. designed the research, analysed the data and wrote the manuscript. P.P. performed the experiments.

### **Additional Information**

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